



Ευρωπαϊκή Ένωση
Ευρωπαϊκό Κοινωνικό Ταμείο



ΕΠΙΧΕΙΡΗΣΙΑΚΟ ΠΡΟΓΡΑΜΜΑ
ΕΚΠΑΙΔΕΥΣΗ ΚΑΙ ΔΙΑ ΒΙΟΥ ΜΑΘΗΣΗ
επένδυση στην κοινωνία της γνώσης

ΥΠΟΥΡΓΕΙΟ ΠΑΙΔΕΙΑΣ & ΘΡΗΣΚΕΥΜΑΤΩΝ, ΠΟΛΙΤΙΣΜΟΥ & ΑΘΛΗΤΙΣΜΟΥ
ΕΙΔΙΚΗ ΥΠΗΡΕΣΙΑ ΔΙΑΧΕΙΡΙΣΗΣ

Με τη συγχρηματοδότηση της Ελλάδας και της Ευρωπαϊκής Ένωσης



Technical University of Crete
Electronics & Computer Engineering Dept.
Electronics Laboratory
Optoelectronics Group

IN VIVO MOLECULAR IMAGING OF EPITHELIAL PRE-CANCERS BASED ON DYNAMIC OPTICAL SCATTERING MODELING

George Papoutsoglou

INTRODUCTION

Motivation

Emerging technologies

Dynamic Contrast-Enhanced Optical Imaging (DCE-OI)

Clinical evidence

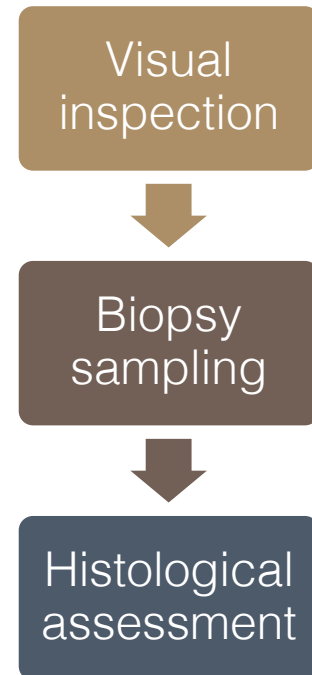
Scope

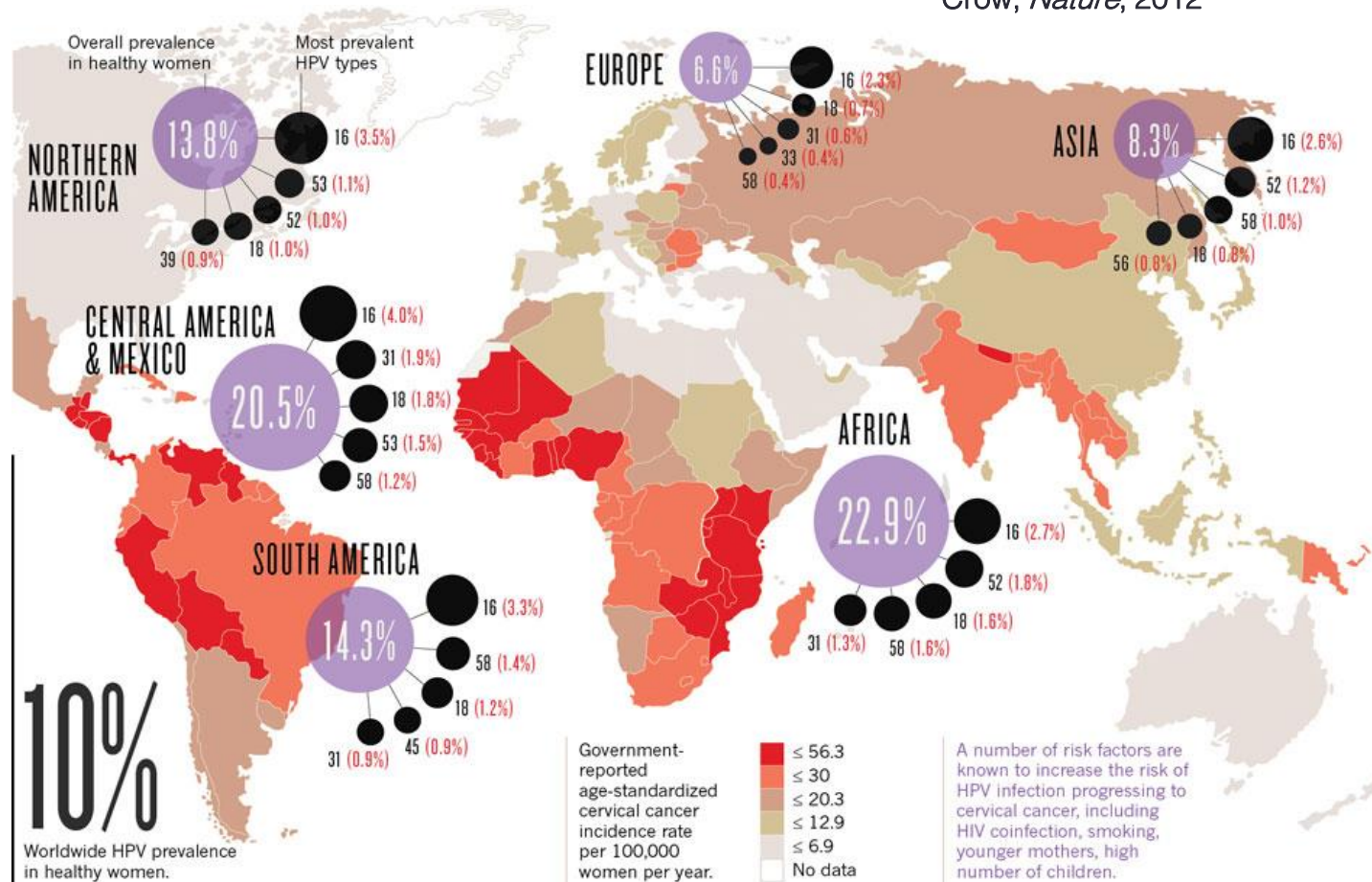
Outline of the project

Motivation

Problems in current diagnostic chain for the early detection of cancer lesions

- Qualitative
- Subjective
- High inter-observer disagreement
- limited diagnostic performance at each step
- additional steps increase complexity and costs



Crow, *Nature*, 2012

- Developed world
 - ▣ poor cost-effectiveness
- Low resource countries
 - ▣ inability to implement and sustain such complicated prevention programs

Dynamic Contrast-Enhanced Optical Imaging (DCE-OI)

Introduced for the first time by C. Balas in the late 90's

C. J. Balas, et al., "In vivo detection and staging of epithelial dysplasias and malignancies based on the quantitative assessment of acetic acid-tissue interaction kinetics," J. Photochem. Photobiol. B-Biology, vol. 53, no. 1-3, pp. 153-157, 1999.

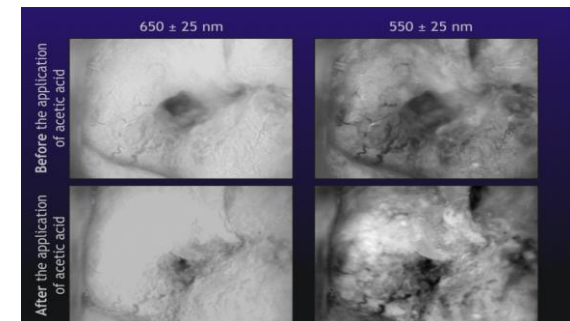
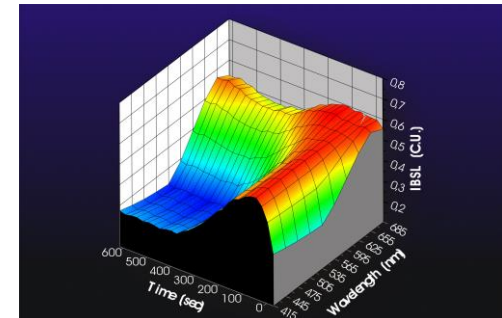
C. Balas, "A novel optical imaging method for the early detection, quantitative grading, and mapping of cancerous and precancerous lesions of cervix," IEEE Trans Biomed Eng, vol. 48, no. 1, pp. 96-104, 2001.

• Dynamic effects

- Information-rich
- Signal profile: identify false positives
 - Inflammatory tissues
 - Repairing epithelium
 - Metaplasia

• Spectral Imaging

- Discriminate between responsive and non responsive areas
- Assess alterations in light scattering properties of the tissue



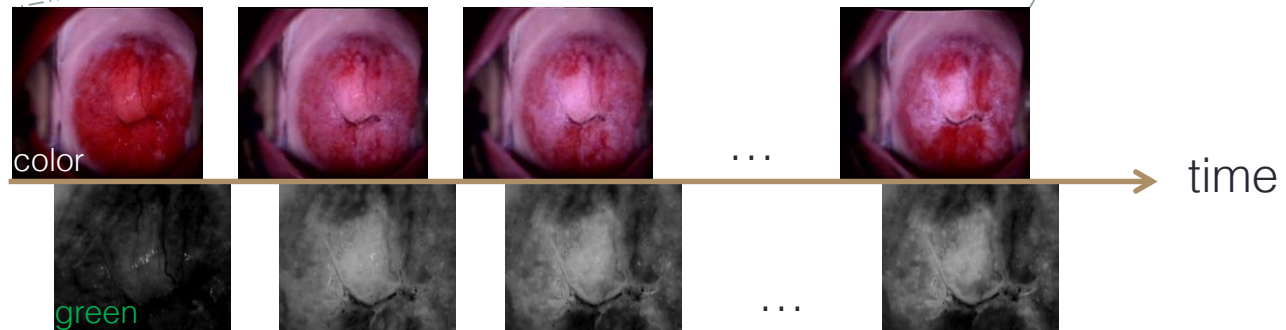
DCE-OI principle

spatio-temporal recording of biomarker-tissue interaction *in-vivo*, **non-invasively** and **in real time**.

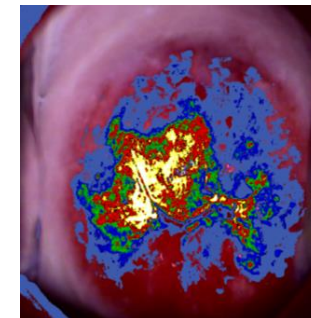
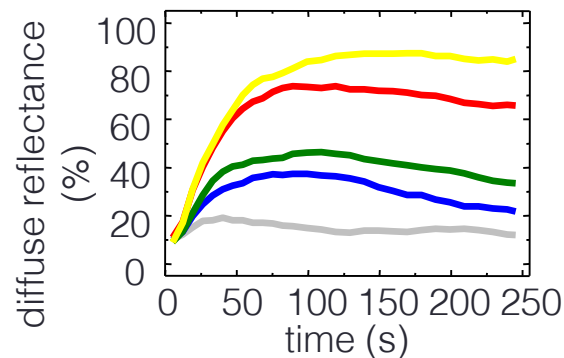
clinical setup



Snapshot
Spectral
Imaging



pixel-by-pixel
recordings



Clinical evidence



Trial profile (Phase II)

Hospitals: Hammersmith (London, UK) St. Mary's (London, UK) Alexandra (Athens, GR)

Aim: To compare the performance of DySIS with the performances of conventional colposcopy and cytology in detecting High Grade CIN

Recruitment: 447 women with abnormal smear

	DySIS	Conventional Colposcopy	Referral Cytology
Sensitivity	79%	49%	53%
Specificity	76%	89%	86%
Diagnostic Odds Ratio	11.81	7.91	6.88

Technology awareness

- **Standard care worldwide**

- Europe
 - CE-Marked
 - Greece, UK, Netherlands, Sweden, France, ...
- USA
 - FDA approval, 2011

- **Prizes**

- Medilink Innovation Award, 2013
- Scottish Life Science Award, 2013



Integrates the most promising sciences

- Molecular Imaging
 - Imaging of specific tissue-marker interactions
- Spectral Imaging
 - Using specific color bands for enhanced imaging
- Dynamic Imaging
 - Recording the changes of tissue characteristics over time



..... without changing screening standard procedures

Going one step further

Exact origins of the phenomenon had been largely unknown

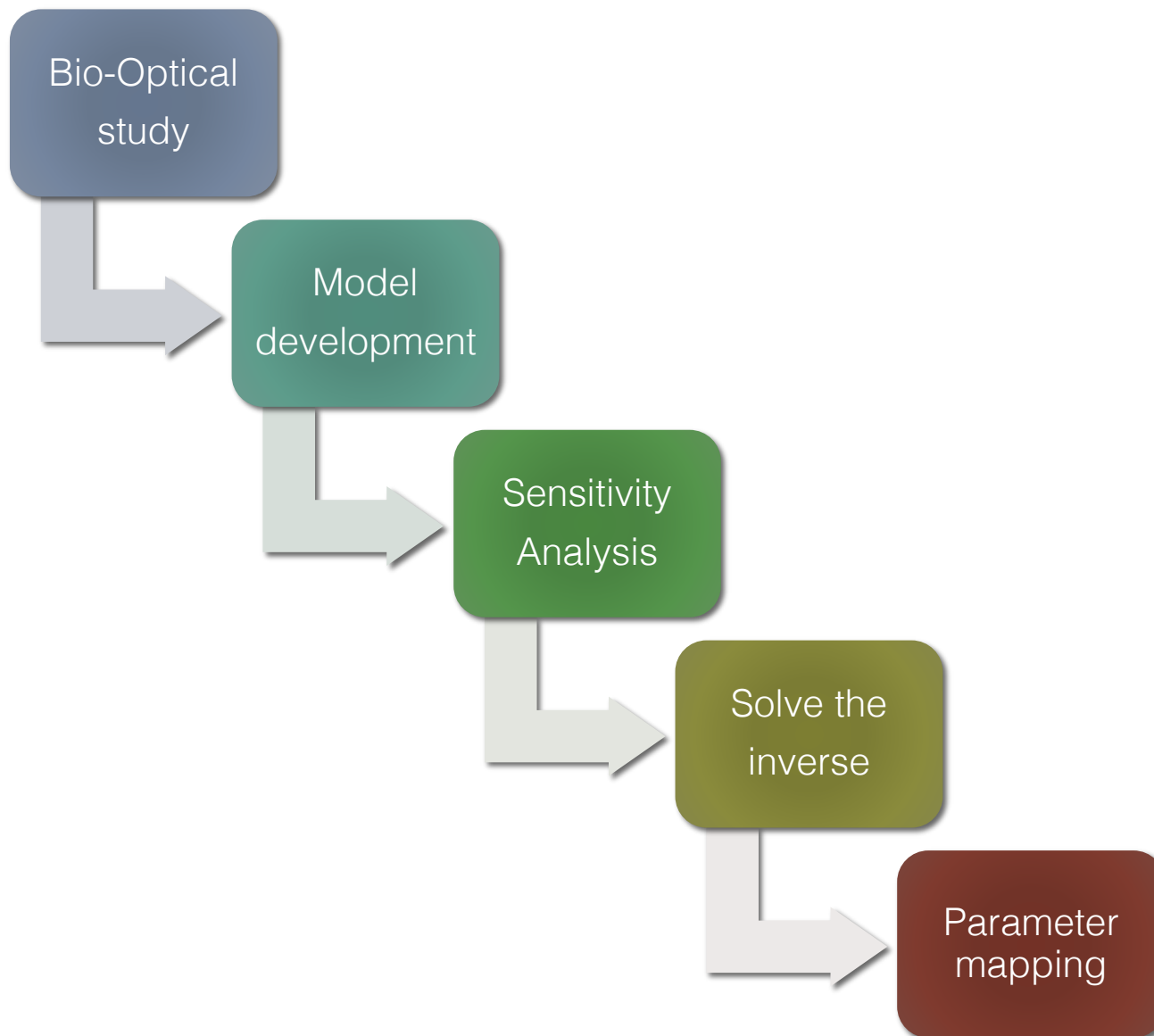
DCE-OI

- Dynamic optical signals are correlated with neoplasia progression
- Dynamic effects are information-rich
 - Transport pathways
 - Reversible pharmacodynamics
- Renders possible the systematic, model-based quantitative assessment of several biological parameters that are determining the features of the experimental data

Scope

- Interpret and correlate the optical phenomenon with the underlying functional and structural alterations
 - Mine diagnostic information by solving the inverse problem
-

Project pipeline



BACKGROUND, STATE OF THE ART

Strategy for modeling metabolic systems

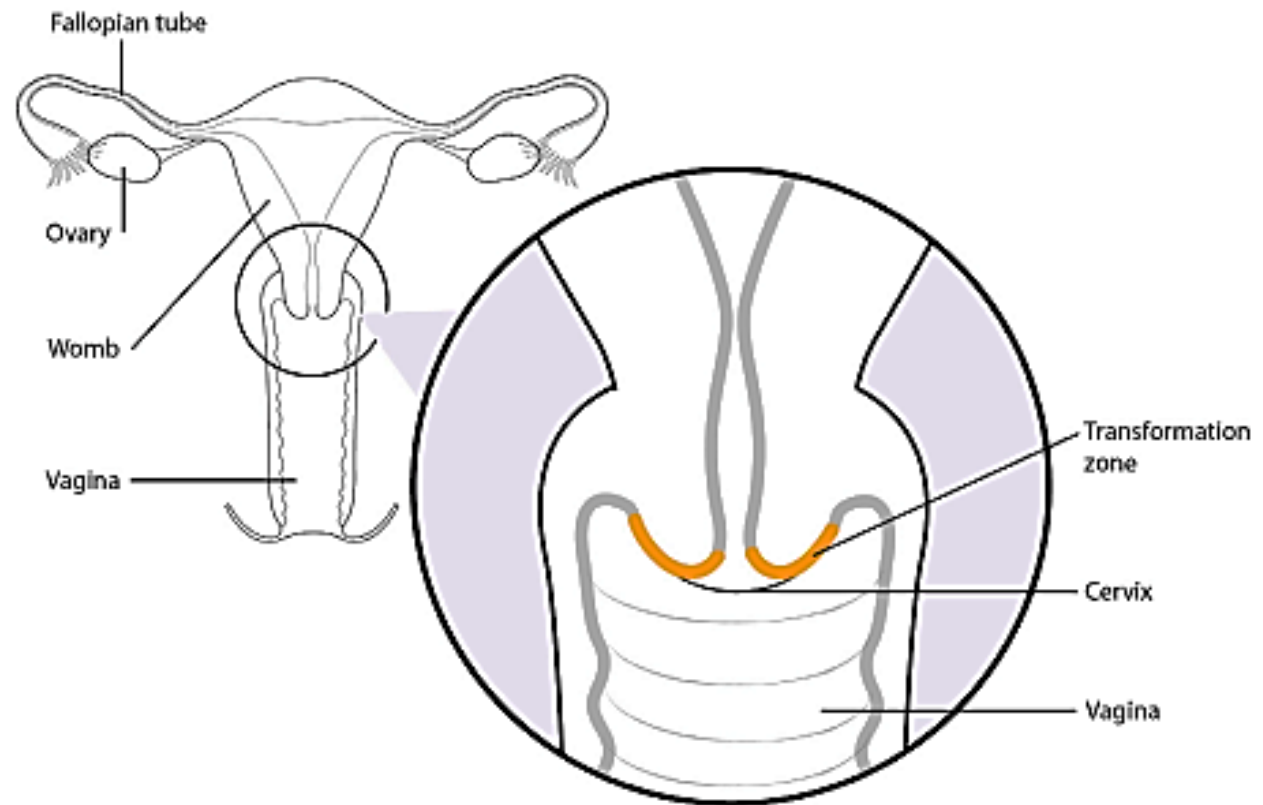
Epithelial pharmacodynamics/pharmacokinetics

Identifiability

Solution of the inverse problem

Epithelia neoplasia of the cervix

- During a woman's lifespan the **columnar epithelium** of the endocervix is **converted** progressively to **squamous**
- CIN tends to form in the vicinity of the Transformation Zone (TZ).



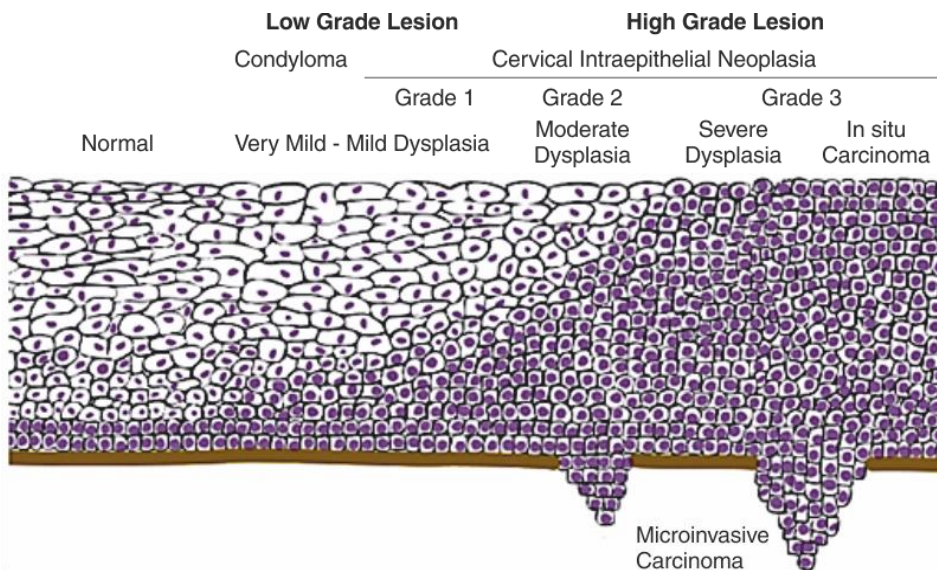
Structural and functional changes during CIN

• Structural changes

- tissue homogenization
- smaller cell size
- larger nuclei
- larger extracellular space

• Functional changes

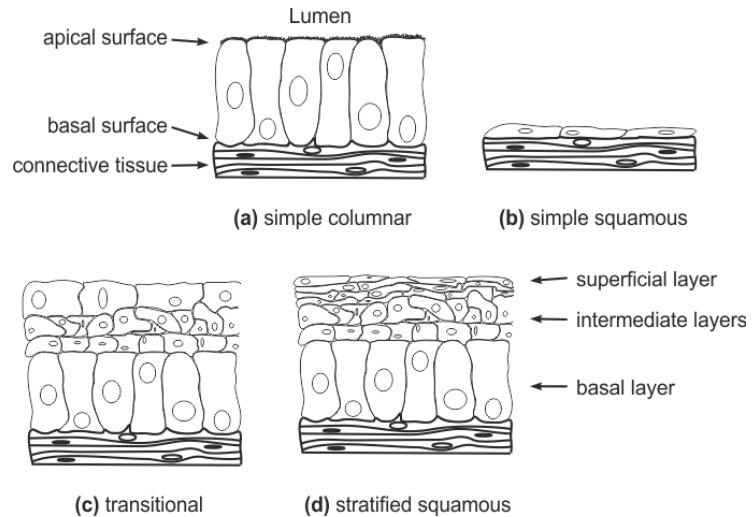
- increased production and proliferation rate
- Tight Junctions
 - greater diffusivity
- Gap Junctions
 - reduced cell-to-cell cross talking
 - quit metabolic cooperation
- pH regulation
 - low extracellular pH
 - normal intracellular pH



The tissue in terms of structure and function

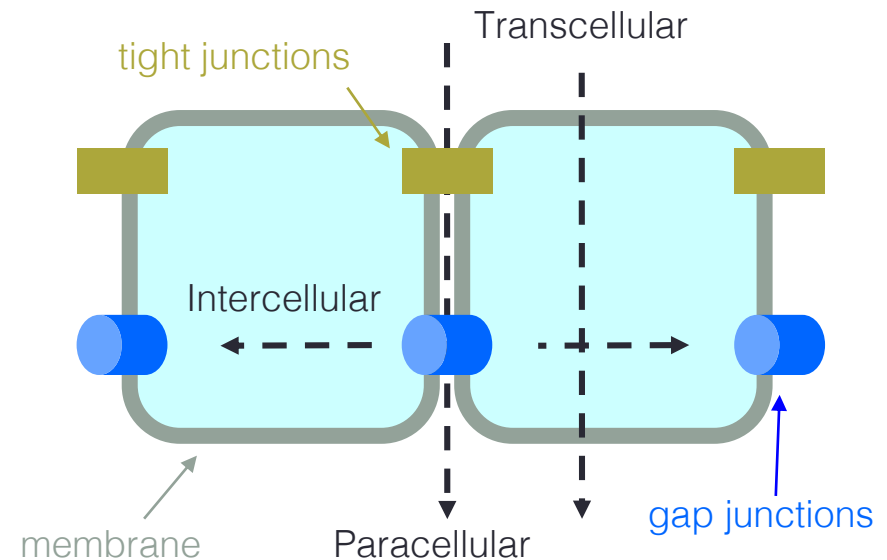
Classification

- Columnar
- Squamous
- Transitional
- **Stratified squamous**



Adhesion and communication

- Plasma membrane
 - Secretion-Absorption: **transcellular**
 - Diffusion: Passive, Active
- Tight junctions
 - Protection: **paracellular**
 - Diffusion: Passive, Size and charge selective
- Gap junctions
 - Communication - Metabolic cooperation: **intercellular**
 - Diffusion: Passive, Size and charge selective



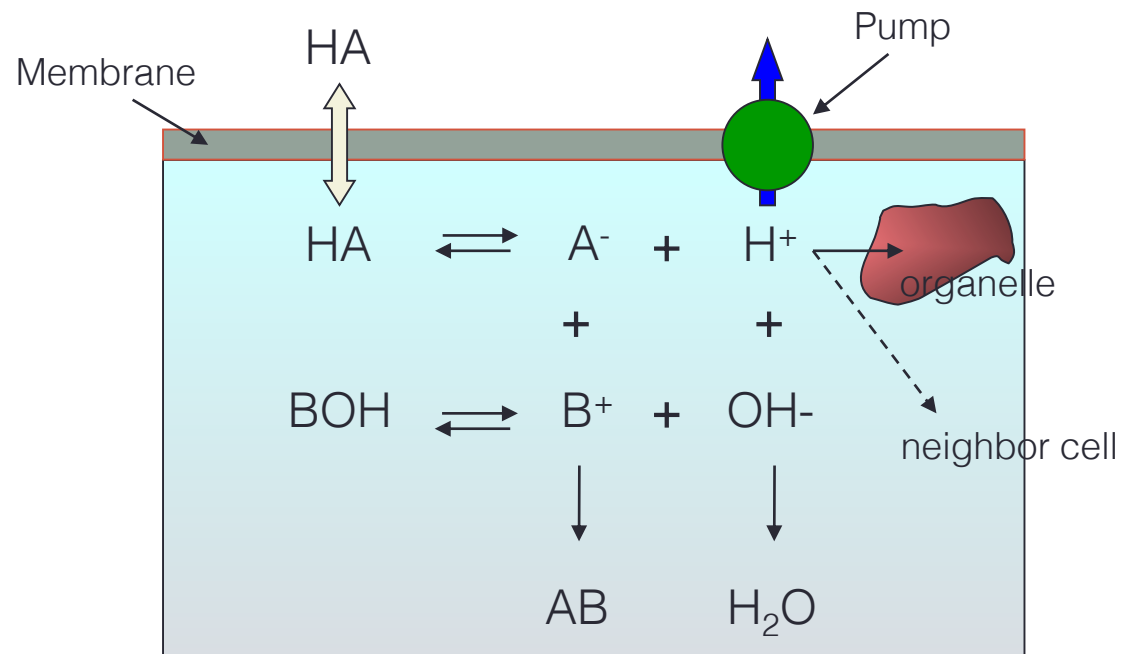
Maintaining the pH

- **Short-term mechanisms**

- physicochemical buffering
- metabolism:
 - organelles
 - metabolic cooperation

- **Long-term mechanisms**

- Ion pumps



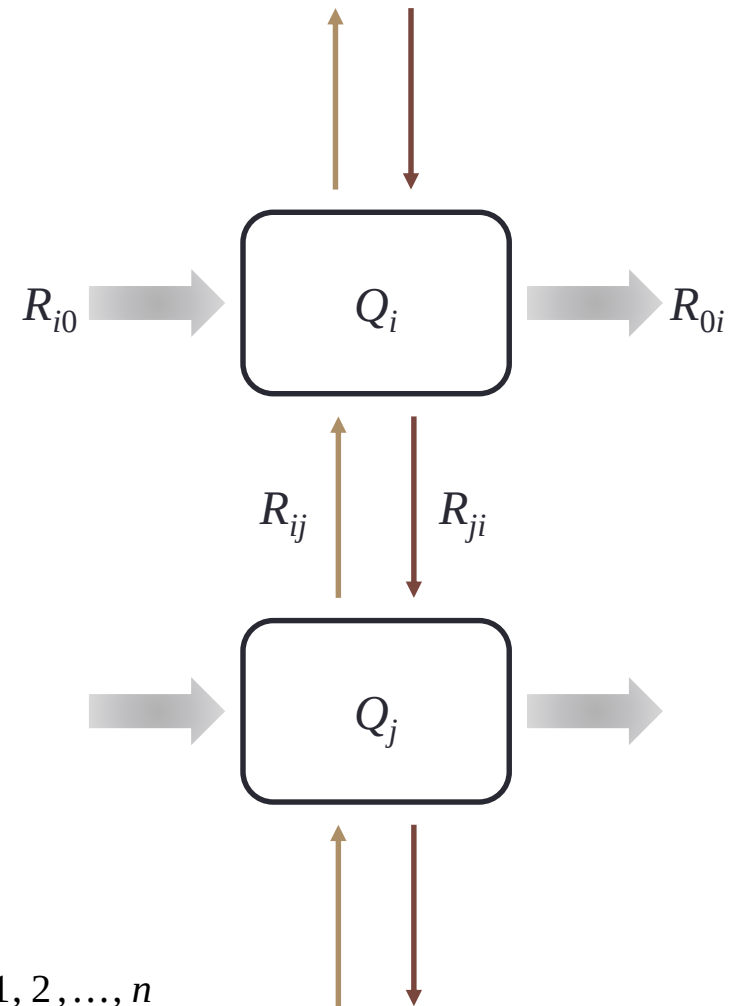
Mathematical representation

Compartmental models

- clustering of the spatially distributed similar information in a tractable discrete topology
- deterministic
- linear or non-linear

interconnection = material flux

- transport from one location to another (diffusion)
- chemical reaction/transformation



Conservation law

$$\frac{dQ_i}{dt} = R_{i0} + \sum_{\substack{j=1 \\ j \neq i}}^n R_{ij} - \sum_{\substack{j=1 \\ j \neq i}}^n R_{ji} - R_{0i}, \quad i = 1, 2, \dots, n$$

Biophysical Laws

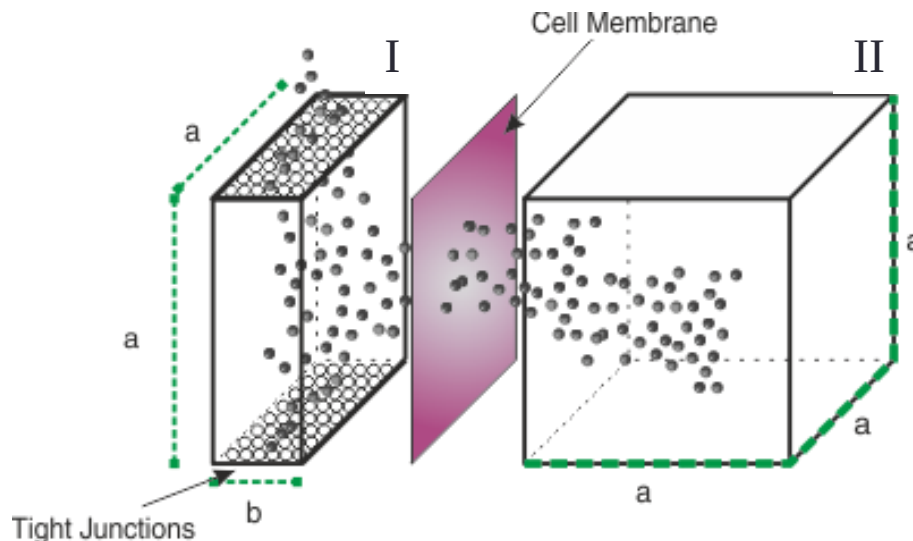
flux = mobility $\times$ concentration $\times$ driving force $\rightarrow J^{(s)} = U^{(s)} C^{(s)} \left(- \frac{d\mu^{(s)}}{dx} \right)$

Fick's first law

$$J_{I \rightarrow II}^{(s)} = P^{(s)} ([S]^I - [S]^II)$$

Goldman-Hodgkin-Katz (GHK) equation

$$J_{I \rightarrow II}^{(s)} = \frac{z_s F V_m}{RT (1 - e^{-z_s F V_m / RT})} P^{(s)} ([S]^I - [S]^II e^{-z_s F V_m / RT})$$



- ▣ Constant flux over a given surface area (A)
- ▣ Constant concentration over a volume (V)

$$\frac{dc}{dt} = - \frac{A}{V} J$$

Towards the solution of the inverse problem

- ✓ Strong biological background
 - ✓ Suitable model
- } address the inverse problem (parameter estimation), directly

Caveat

- uncertain model structure and/or parameters
- mathematically interacting and/or correlated parameters

Question:

Can the unknown system parameters be uniquely estimated from the available experimental data and using the proposed model's structure?

Theoretical study

- sensitivity
 - identifiability
 - estimability
- }
 - reduce the parameter complexity
 - improve the posedness of the inverse problem.

Parameter identifiability

- **Parameter types**

- **Structural**: inherent to the structural equations
- **Experimental**: imposed by experimental conditions
- **Observational**: captured by the observations

- **Global identifiability**

- **Observational** $\equiv$ **Structural**
(unique)
- linear models
 - algebraic manipulations
 - transformations (Laplace, similarity transformations)
- non-linear models
 - Differential algebra
 - Expansions (Taylor series, Lie derivatives)

- **Local identifiability**

- **Observational** $\subset$ **Structural**
(not unique)
- Local sensitivity analysis
- Global Sensitivity Analysis
 - Model reduction/restructuring
 - Parameter ranking

Sensitivity analysis in dynamic system models

Local sensitivity analysis

1. derivative at a “base point”
2. local sensitivity matrix (Jacobian)

$$\mathbf{S}_D = \begin{bmatrix} \left. \frac{\partial \hat{\mathbf{y}}}{\partial p_1} \right|_{t_1} & \dots & \left. \frac{\partial \hat{\mathbf{y}}}{\partial p_j} \right|_{t_1} \\ \vdots & \ddots & \vdots \\ \left. \frac{\partial \hat{\mathbf{y}}}{\partial p_1} \right|_{t_s} & \dots & \left. \frac{\partial \hat{\mathbf{y}}}{\partial p_j} \right|_{t_s} \end{bmatrix}$$

3. parameter assessments
 - Linear (e.g. Pearson's)
 - Principal Component Analysis (PCA)
 - Fisher Information Matrix (FIM)

Global sensitivity analysis

- parameters → **random variables**
- No analytic in/output relationship and/or model additivity is required

- **Variance-based methods**

- decompose the output variance into terms of increasing dimensionality:

$$V(Y) = \sum_{i=1}^N V_i + \sum_i \sum_j V_{ij} + \sum_i \sum_j \sum_k V_{ijk} + \dots + V_{1,2,\dots,k}$$

- robust statistical inferences
- condensed format

First Order Sensitivity (FOS):

$$S_i = V_i / V(Y)$$

Total Order Sensitivity (TOS):

$$S_{Ti} = S_i + S_{ij} + \dots + S_{ij..k}$$

Method of Sobol'

- **Conditional variances as multidimensional integrals**
- **Quasi - Monte Carlo procedure:**
 1. Generate a $N_{\text{sample}} \times 2k$ matrix using low discrepancy number sequences e.g. LP_{τ}
 2. Split into a sample ($\mathbf{A}^k$) and a re-sample ($\mathbf{B}^k$) matrix
 3. Form the $\mathbf{A}_B^{(i)}$ and $\mathbf{B}_A^{(i)}$ matrices
 - First order sensitivity (FOS)

$$V_{X_i} \left(E_{\mathbf{X} \sim i} (Y | \mathbf{X}_i) \right) = \frac{1}{N_{\text{sample}}} \sum_{j=1}^{N_{\text{sample}}} f(\mathbf{B})_j \left(f(\mathbf{A}_B^{(i)})_j - f(\mathbf{A})_j \right)$$

- Total order sensitivity (TOS)

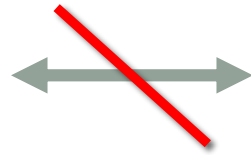
$$E_{\mathbf{X} \sim i} \left(V_{X_i} (Y | \mathbf{X}_{\sim i}) \right) = \frac{1}{2N_{\text{sample}}} \sum_{j=1}^{N_{\text{sample}}} \left(f(\mathbf{A})_j - f(\mathbf{A}_B^{(i)})_j \right)^2$$

Both FOS and TOS indexes have been calculated for every time instance lapsed after the initiation of the phenomenon

Theoretical identifiability analysis

FOS: parameter ranking

high ranking



identifiability

TOS: designate non-essential parameters

- nullity (or inferiority to an empirical threshold)
- non-injectivity

Non-identifiability may be assessed from:

- linear dependence of the TOS with respect to time
 - correlation = ± 1
 - repeatedly remove one unidentifiable parameter each time, until no more unidentifiable parameters remain
 - parameter interactions
-

Parameter estimation

Let the most identifiable parameter set ($\mathbf{p}$) be defined
 Optimization of a cost function (likelihood), $J(\mathbf{p}) = L(\mathbf{p}|\mathbf{z})$

Frequentist approach

Find the set $\mathbf{p}$ that gives the highest probability to the observed data

- assumption on error
- maximum likelihood methods

Special case:

independent, additive Gaussian noise with zero mean and constant variance

$$J(\mathbf{p}) = \sum_{i=1}^{n_y} \sum_{t=t_0}^{t_{\max}} \left(\frac{z_i^*(t) - z_i(t, \mathbf{p})}{\sigma_i} \right)^2$$

Minimization methodologies

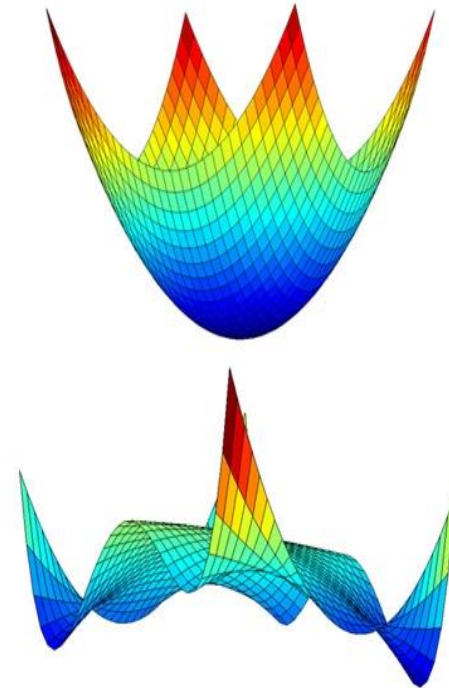
- linear/non-linear least squares
 - heuristic search
-

Global optimization

- **Deterministic strategies**
- **Stochastic strategies**

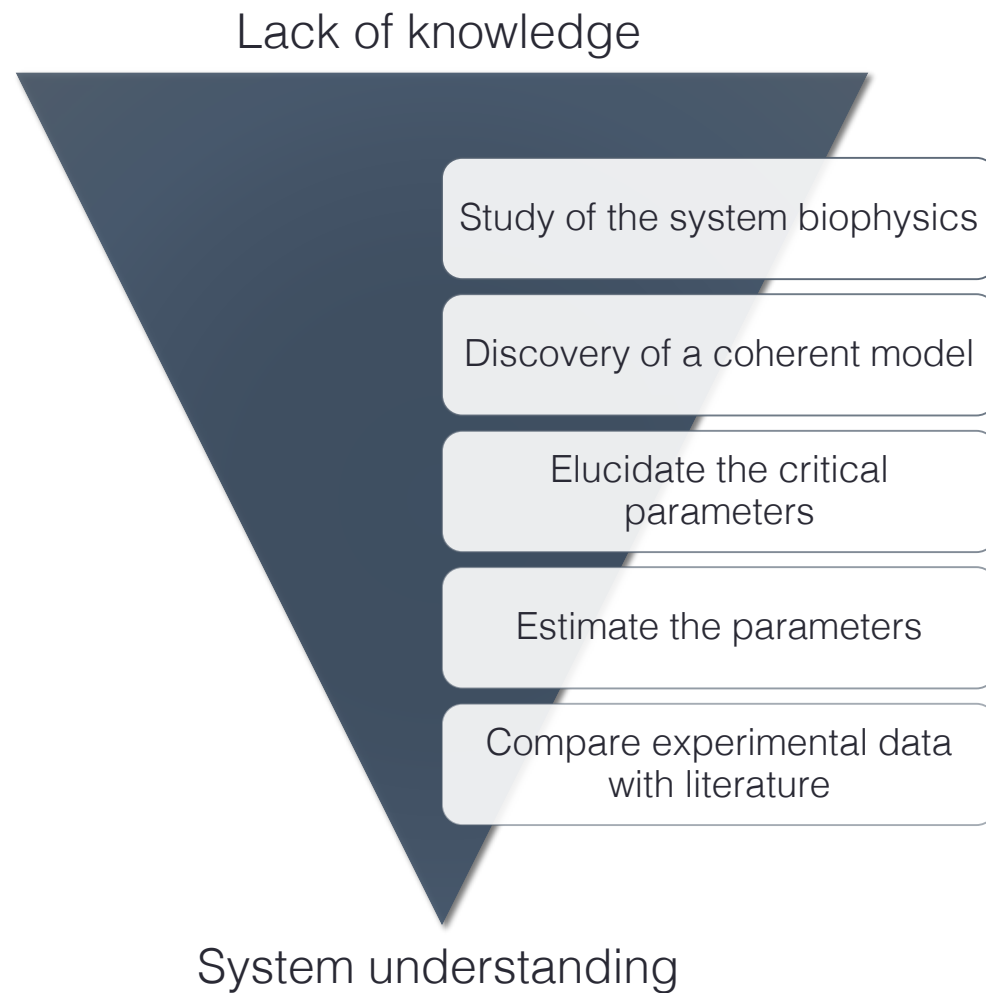
Model: multi-resolution design

- Non-Convex
- no analytical representation
- non factorable equations



direct-search (derivative-free) GO methods are mostly suitable

Roadmap



Bio-Optical study

Mathematical
Implementation

Sensitivity
Analysis

Solve the
inverse

Parameter mapping

THESIS RESULTS & CONTRIBUTIONS

1. BIO-OPTICAL MODEL DESIGN

Biomarker pharmacodynamics

The “ouzo effect”

Interpretation of the optical excitation

Result 1: The origin of the bio-optical phenomenon

- We present the link between metabolic processes, biomarker pharmacodynamics/kinetics and the provoked dynamic, macroscopic phenomenon
- The phenomenon's dynamics is not determined by the intrinsic time characteristics of the conformational changes, but from the dynamic characteristics of the change causing factor instead.

Relevant publications

C. Balas, G. Papoutsoglou, and A. Potirakis, "*In vivo molecular imaging of cervical neoplasia using acetic acid as biomarker*," IEEE J. Sel. Top. Quantum Electron., vol. 14, no. 1, pp. 29-42, 2008

Biophysical interpretation of phenomenon

● : H^+ ● : Acetate $^-$



: gap junctions, inactive in CIN

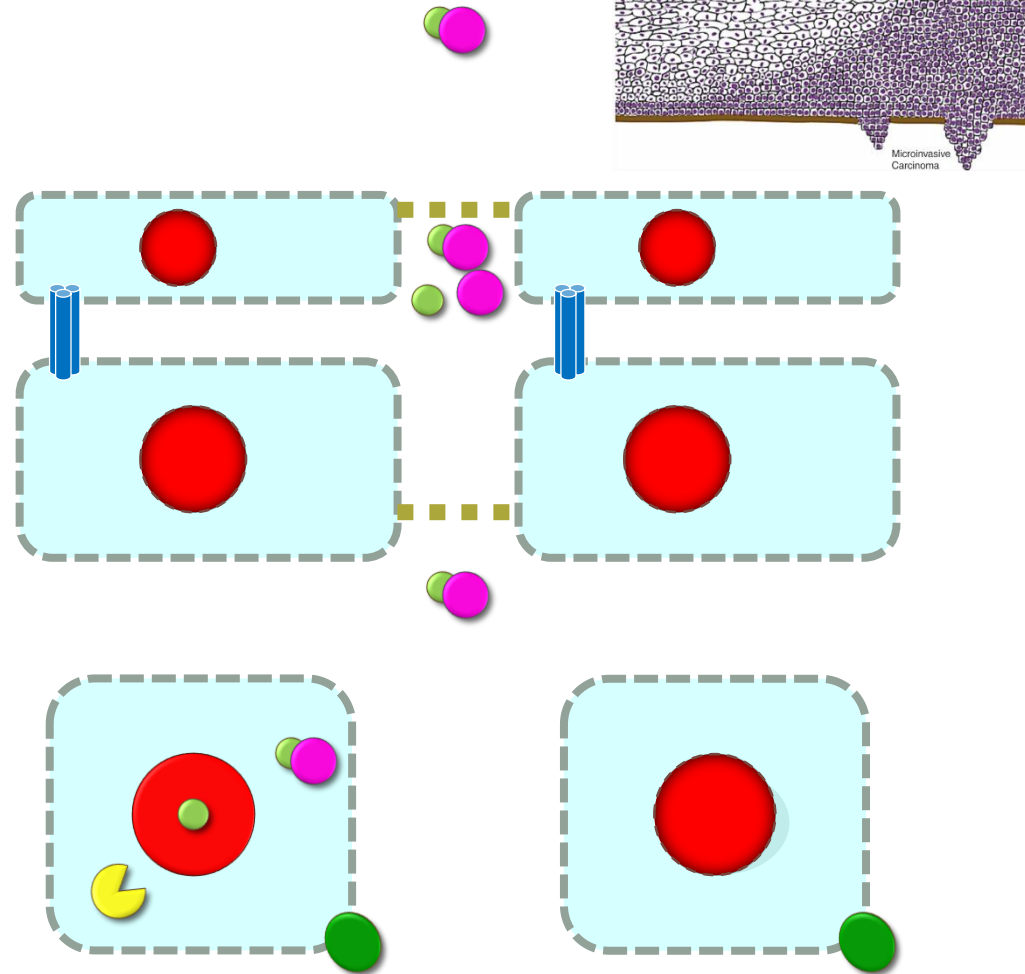
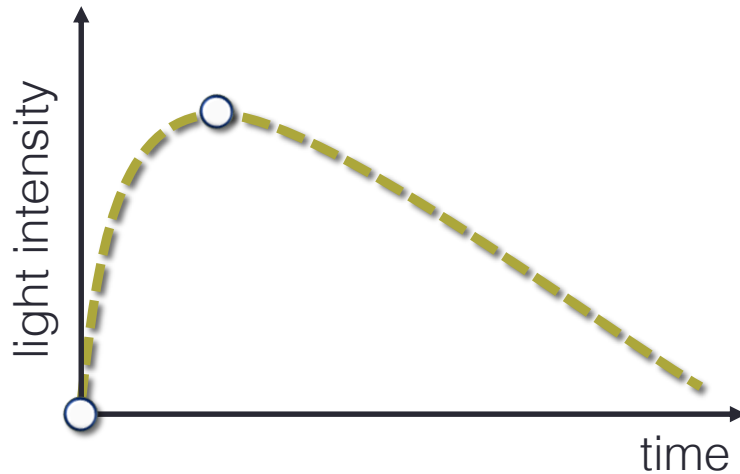
--- : tight junctions, loose in CIN



: ion buffers



: pumping mechanisms



Optical properties of normal and atypical tissue

Normal epithelium is transparent

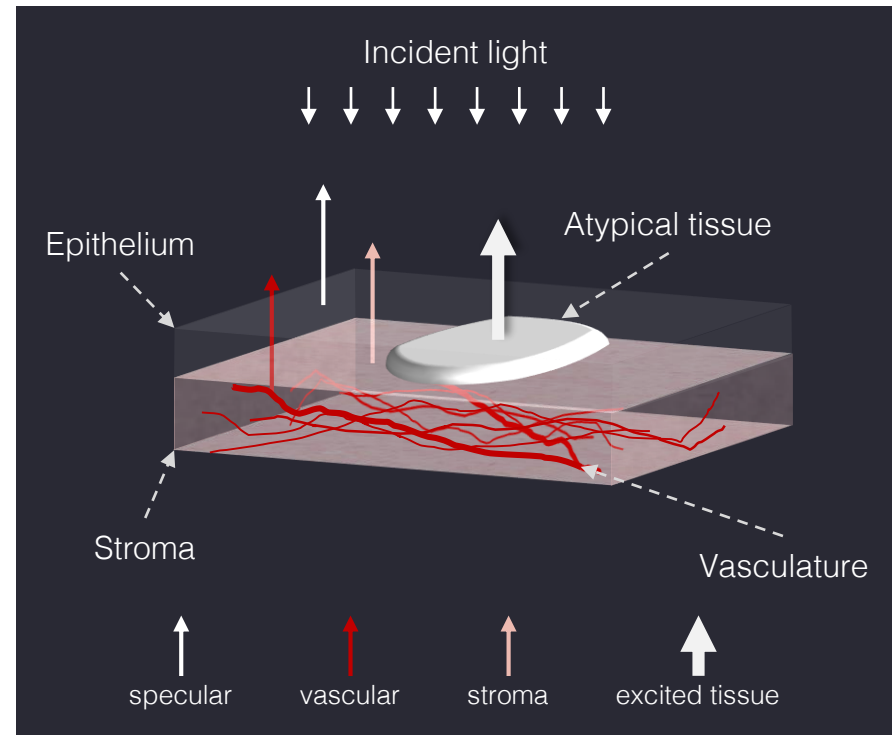
- Forward (Mie) scattering
 - Nucleus
 - Cell
- Fresnel reflection
- **Backscattering/Absorption**
 - Stroma
 - Vasculature



the “ouzo effect”

Atypical, acetic acid-treated epithelium acts as a diffuser

- Strong backscattering



The backscattered photon increase accrues to small-sized-AA-induced cellular components in the cytoplasm and the nucleus. (Wu, et al., Optics Express, 2005)

Result 1: The origin of the bio-optical phenomenon

- **Road to acetowhitening:**

- ionization (pH drop)
 - protein denaturation
 - cytoplasmic component coagulation
 - change in the refractive index of the cell
 - alteration in the light scattering characteristics of the tissue
 - acetowhitening!
- } $\mu\text{s/ns}$ regime
(Finkelstein, *Phys. Life. Rev.*, 2004) $\ll 4\text{mins}$

The phenomenon's dynamics are not determined by the intrinsic time characteristics of the conformational changes, but from the dynamic characteristics of the change causing factor instead.

The development of a biophysical model of the biomarker kinetics allows for the quantitative assessment of several biological parameters that are determining the features of the experimental data.

Conceptualization

Model development

Sensitivity
Analysis

Solve the
inverse

Parameter mapping

THESIS RESULTS & CONTRIBUTIONS

2. MATHEMATICAL FRAMEWORK

Differential equation system

Model parameters

Input-Output

Preliminary validation

Result 2: Model development and preliminary validation

- **Formulation of a coherent model of the system under study**
- **Validation**
the biomarker kinetics and the effect's temporal characteristics are correlated with the histological features used to grade biopsy samples
- **Model-based fitting is possible**

Relevant publications

C. Balas, G. Papoutsoglou, C. Loukas, Y. Skiadas, C. Pappas, D. Haidopoulos, E. Diakomanolis, and W. P. Soutter, "*In vivo assessment of microstructural and functional alterations in cervical neoplasia*," in Conference proceedings: European Conferences on Biomedical Optics (ECBO), 2009.

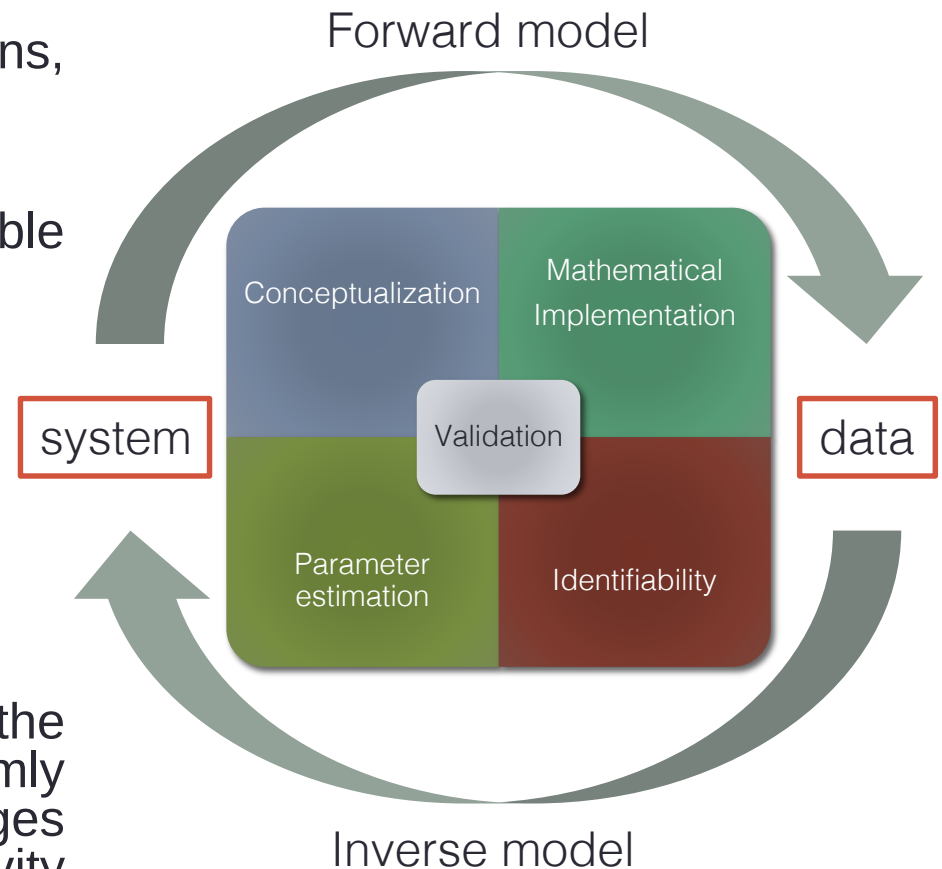
Model building strategy

Conceptualization

- Modeling purpose
- Assumptions (aggregations, idealizations, etc.)
- **Mathematical framework**
 - Input-output parameter/variable relationship
 - bio-chemical/physical laws
- **Parameter identifiability**
 - Model reduction
 - Model restructuring
- **Parameter estimation**

Validation

An integral component of the modeling process, being firmly embedded within all its stages rather than merely being an activity carried out once model identification has been completed



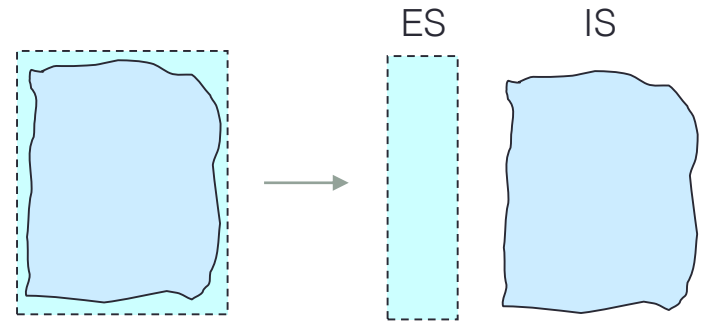
Mathematical framework

We assume that each individual cell constitutes a two-compartmental system

1st compartment: cell (IS)

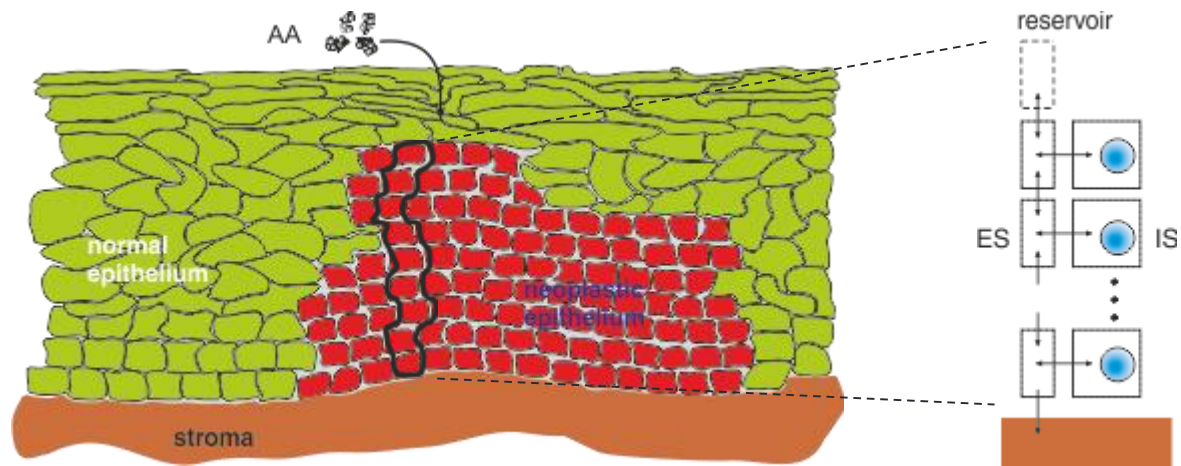
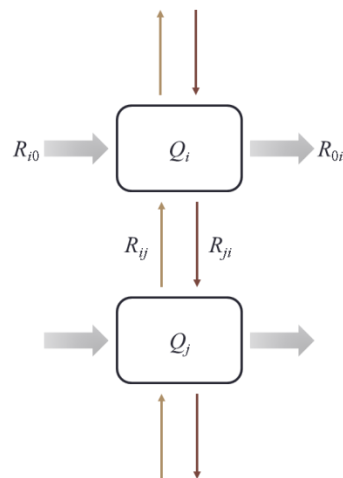
2nd compartment: extracellular space (ES)

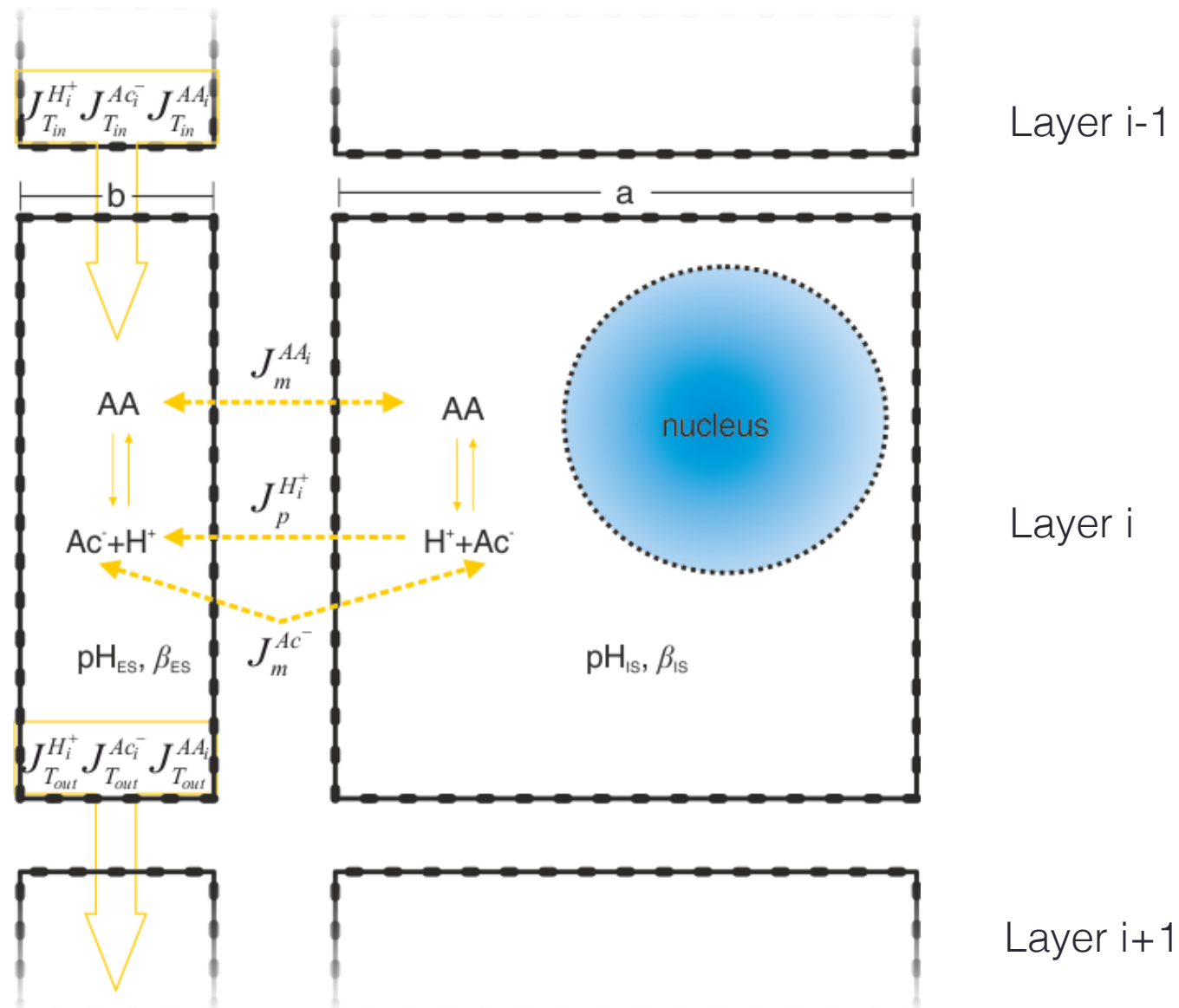
buffered, well-stirred, kinetically homogeneous



- Uniform distribution of cells
- CIN progression is proportional to the number of layers

stack of two-compartmental cell systems



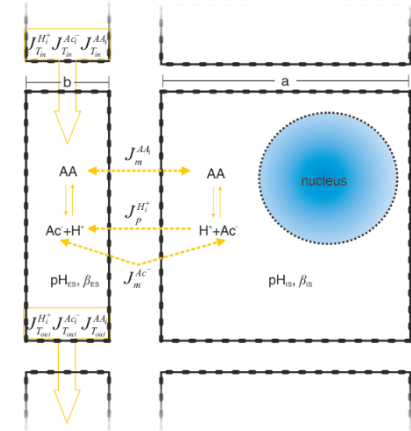


Differential equation system

Intracellular Space

$$\dot{[TA]}_{IS}^i = \rho_{IS} (J_m^{AA_i} + J_m^{Ac_i})$$

$$\dot{[H]}_{IS}^i = -\ln 10 [H]_{IS}^i \rho_{IS} (\beta_{IS})^{-1} (\varphi_{IS}^i J_m^{AA_i} - \omega_{IS}^i J_m^{Ac_i} - J_p^{H_i})$$



Extracellular Space

$$\dot{[TA]}_{ES}^i = \rho_{ES} (J_m^{AA_i} + J_m^{Ac_i}) + \rho_{TJ} g_{TJ} (J_{TJ}^{AA_{i-1}} - J_{TJ}^{AA_{i+1}} + J_{TJ}^{Ac_{i-1}} - J_{TJ}^{Ac_{i+1}})$$

$$\dot{[H]}_{ES}^i = -\ln 10 [H]_{ES}^i (\beta_{ES})^{-1} \left\{ \rho_{ES} (\varphi_{ES}^i J_m^{AA_i} - \omega_{ES}^i J_m^{Ac_i} - J_p^{H_i}) + \rho_{TJ} g_{TJ} \left[\varphi_{ES}^i (J_{TJ}^{AA_{i-1}} - J_{TJ}^{AA_{i+1}}) + \omega_{ES}^i (J_{TJ}^{Ac_{i-1}} - J_{TJ}^{Ac_{i+1}}) \right] \right\}$$

Reservoir layer: no IS

Fick: $J_{I \rightarrow II}^{(S)} = P^{(S)} ([S]^I - [S]^{II})$

Last layer: $J_{TJ}^{[S]_{i+1}} \rightarrow K_v [S]$

GHK: $J_{I \rightarrow II}^{(S)} = \frac{z_S F V_m}{RT (1 - e^{-z_S F V_m / RT})} P^{(S)} ([S]^I - [S]^{II} e^{-z_S F V_m / RT})$

Mathematical particularities

- **adaptable structure**
 - the number of layers **defines** the number of differential equations that are integrated in the system.
- **dynamic degree of ionization of AA (ω , ϕ)**

$$\omega_{IS}^i = \frac{K_\alpha}{[H]_{IS}^i + K_\alpha + 2.3(\beta_{IS})^{-1} K_\alpha \frac{[H]_{IS}^i}{[H]_{IS}^i + K_\alpha} [TA]_{IS}^i}$$

- **trans-layer voltage (ΔV_{TJ})**

$$\Delta V_{TJ} = \frac{RT}{F} \ln \frac{P_{TJ}^{(H)} [H]_{ES}^{i-1} + P_{TJ}^{(Ac)} [Ac]_{ES}^i}{P_{TJ}^{(H)} [H]_{ES}^i + P_{TJ}^{(Ac)} [Ac]_{ES}^{i-1}}$$

- **proton pumping rate**

$$J_p(pH_{IS}) = \begin{cases} \frac{K_p}{pH_{IS,K_p} - 7.4} pH_{IS}, & pH_{IS} > pH_{IS,K_p} \\ K_p, & pH_{IS} = pH_{IS,K_p} \\ \frac{K_p}{pH_{IS,K_p} - 6} pH_{IS}, & pH_{IS} < pH_{IS,K_p} \end{cases}$$

- **[H] to pH conversion**

$$\frac{d[H]_{IS}^{IS}}{dt} = - \frac{2.303}{\beta_{IS}} [H]_{IS} \frac{(dQ_H)^{IS}}{dt}$$

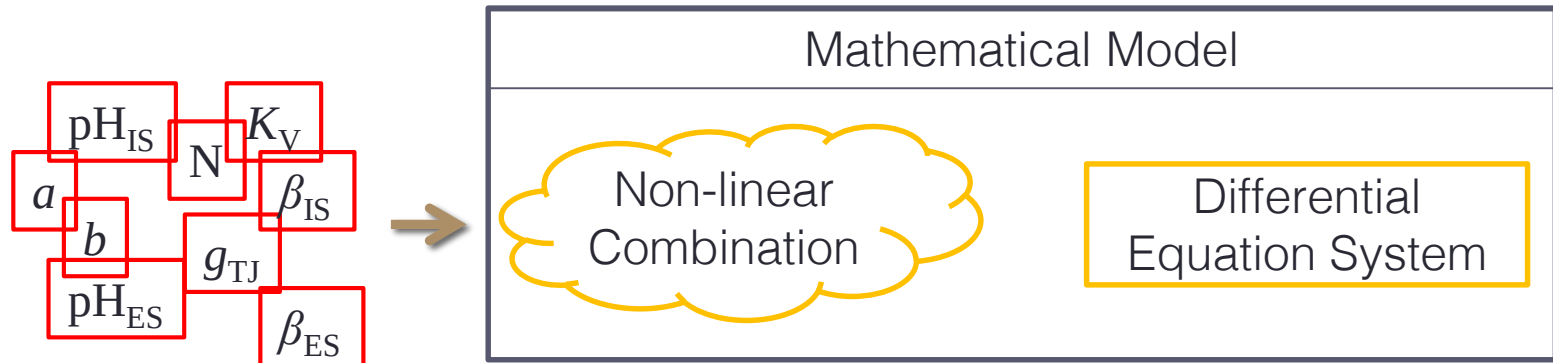
Model: multi-resolution design

- no single analytical representation
- model equations are not factorable or/and cannot anyhow be algebraically manipulative

Model biological parameters

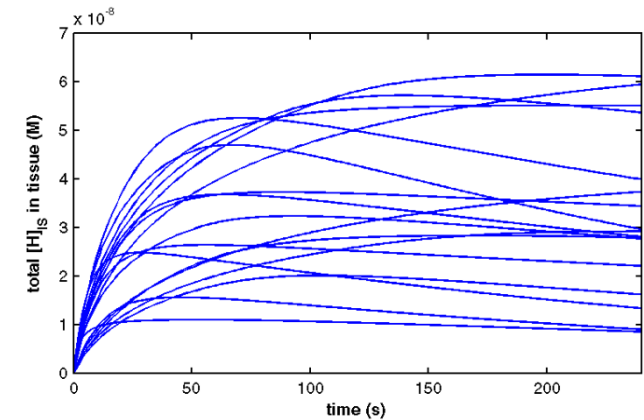
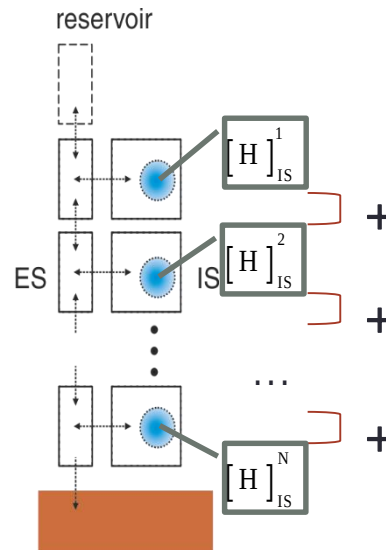
	Parameter	Epexegesis
Structural	a^3	volume (in μm^3) of the IS – V_{IS}
	$a^2 \times b$	volume (in μm^3) of the ES – V_{ES}
	a^2	cell diffusion area (in μm^2) – A_{m}
	$a \times b$	TJ diffusion area (in μm^2) – A_{TJ}
	N	number of epithelial neoplastic layers
Functional	β_{IS}	IS intrinsic buffering capacity
	β_{ES}	ES intrinsic buffering capacity
	pH_{IS}	IS pH
	pH_{ES}	ES pH
	$\text{pH}_{\text{IS,Kp}}$	pH level in which the H^+ pump activity maximizes
	g_{TJ}	TJ porosity factor
	K_{V}	solute diffusion rate at the tissue-stroma interface
	$P^{(\text{S})}$	solute permeabilities
	$\Delta V_{\text{TJ}}, \Delta V_{\text{m}}$	transmembrane voltage gradient (TJ and cell's membrane)

Input-output

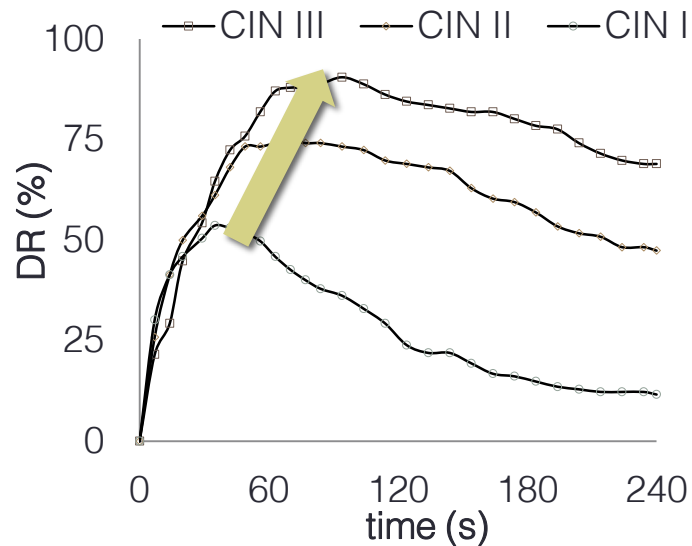


the intracellular H^+ concentration vs. time curve is the model's **output**

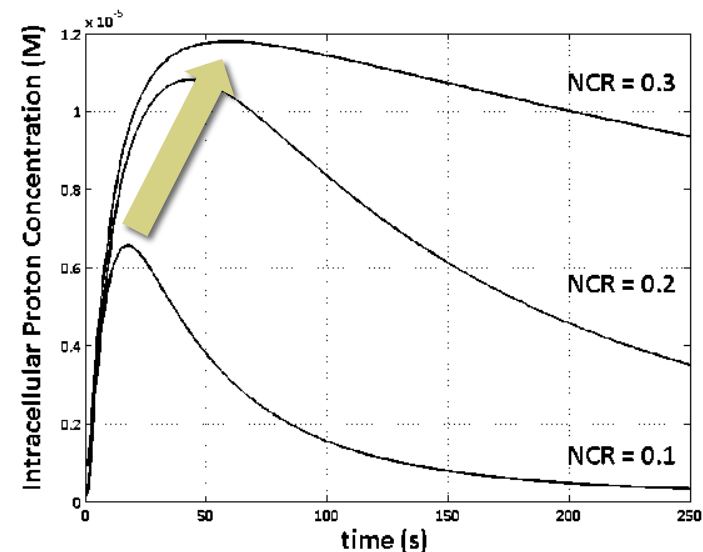
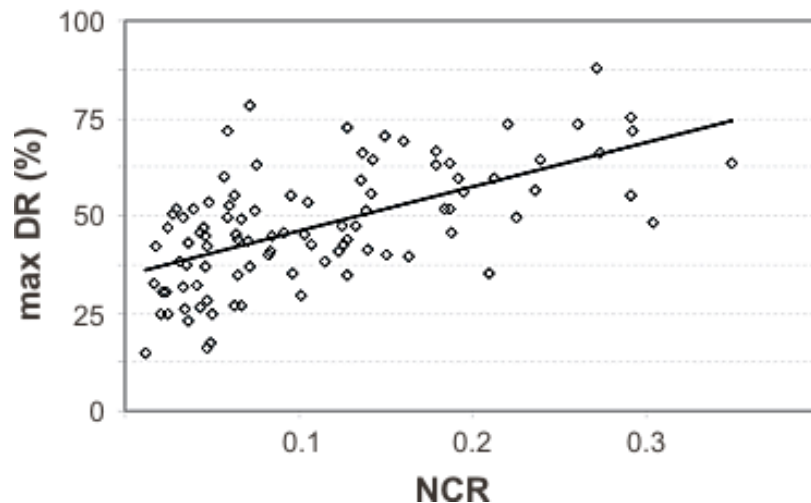
$$y^M(t) = \sum_{i=1}^N \left\{ [\text{H}]_{\text{IS}}^i(t) - [\text{H}]_{\text{IS}}^i(0) \right\}$$



Result 2: Preliminary validation of the developed model



- the biomarker kinetics and the AW characteristics are correlated with the histological features used to grade biopsy samples



Result 2: Model development and preliminary validation

- **Neoplasia development imposes a series of structural and functional alterations**
 - **Clear correlation between the dynamic scattering characteristics of the optical effect and model predictions**
 - **Model-based fitting is possible**
 - > calculation of dynamic optical parameters that correlate well with histological features used to grade biopsy samples
-

Conceptualization

Mathematical
Implementation

Sensitivity
Analysis

Solve the
inverse

Parameter mapping

THESIS RESULTS & CONTRIBUTIONS

3. SENSITIVITY ANALYSIS

Model reduction

Validation

Model restructuring

Result 3: Critical, neoplasia-related parameters

- **Parameter reduction**

- K_V : **null** TOS function
- β_{IS} , β_{ES} , pH_{IS} , a : not fulfilling the combined identification criteria

- **key determinants of the model's output**

- Structural: N , b that relate to histology grading
- Functional: pH_{ES} , g_{TJ} that relate to the altered tissue activity

$$\text{FOS: } S_i = V_i / V(Y)$$

$$\text{TOS: } S_{Ti} = S_i + S_{ij} + \dots + S_{ij..k}$$

Relevant publications

1. G. Papoutsoglou, A. Anastasopoulou, G. Stavrakakis, P. Soutter, and C. Balas, "In vivo dynamic imaging, in silico modeling and global sensitivity analysis for the study and the diagnosis of epithelial neoplasia.," in Conference proceedings : Annual International Conference of the IEEE Engineering in Medicine and Biology Society. Boston, USA, 2011, vol. 2011, pp. 95–9
 2. G. S. Papoutsoglou and C. Balas, "Estimation of neoplasia-related biological parameters through modeling and sensitivity analysis of optical molecular imaging data.," IEEE Transactions on Biomedical Engineering, vol. 60, no. 5, pp. 1241–9, May 2013.
-

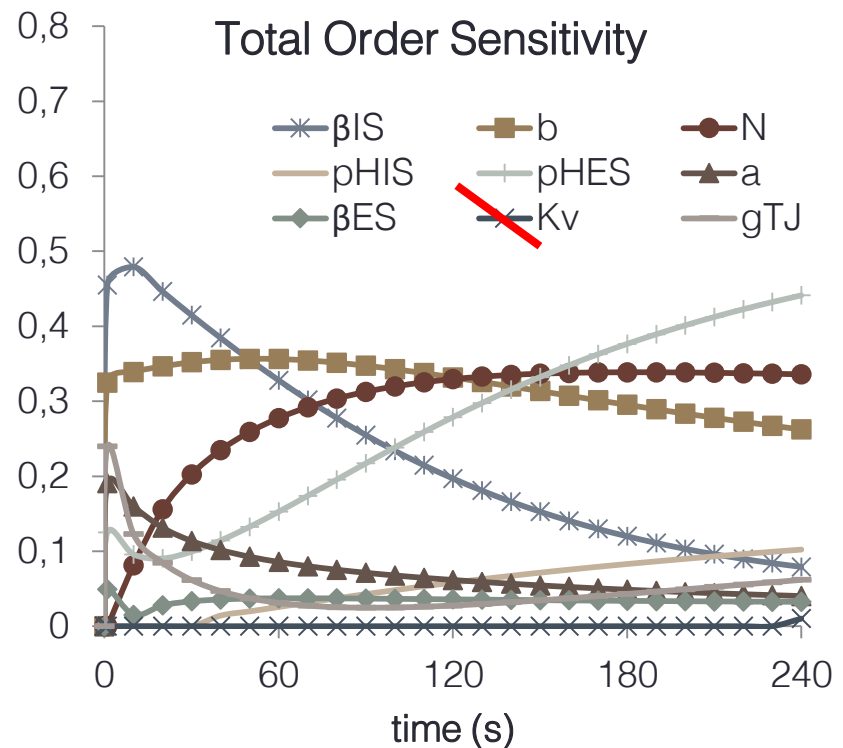
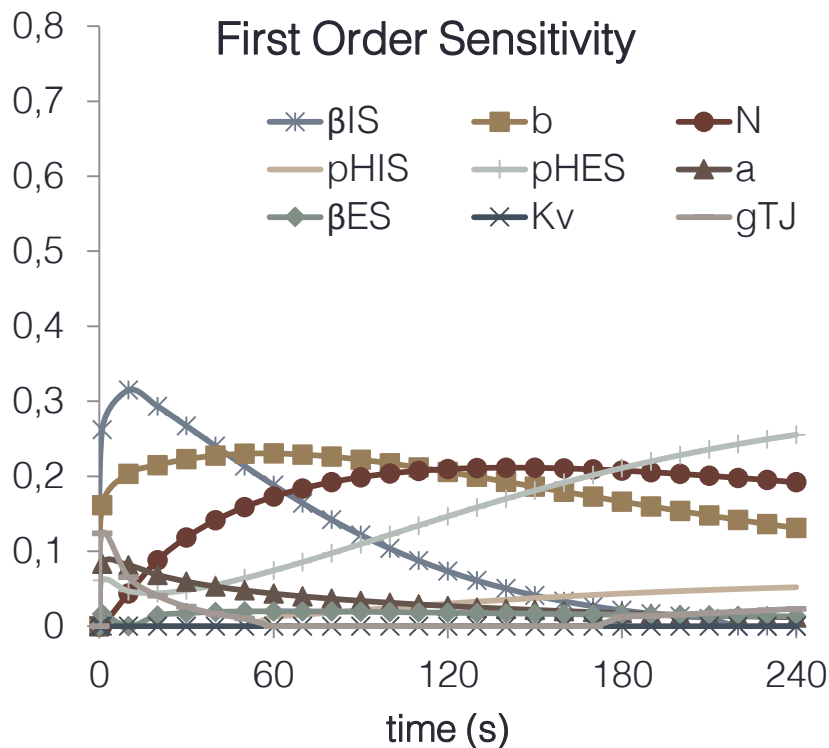
Preliminary global sensitivity analysis results

FOS and TOS depend

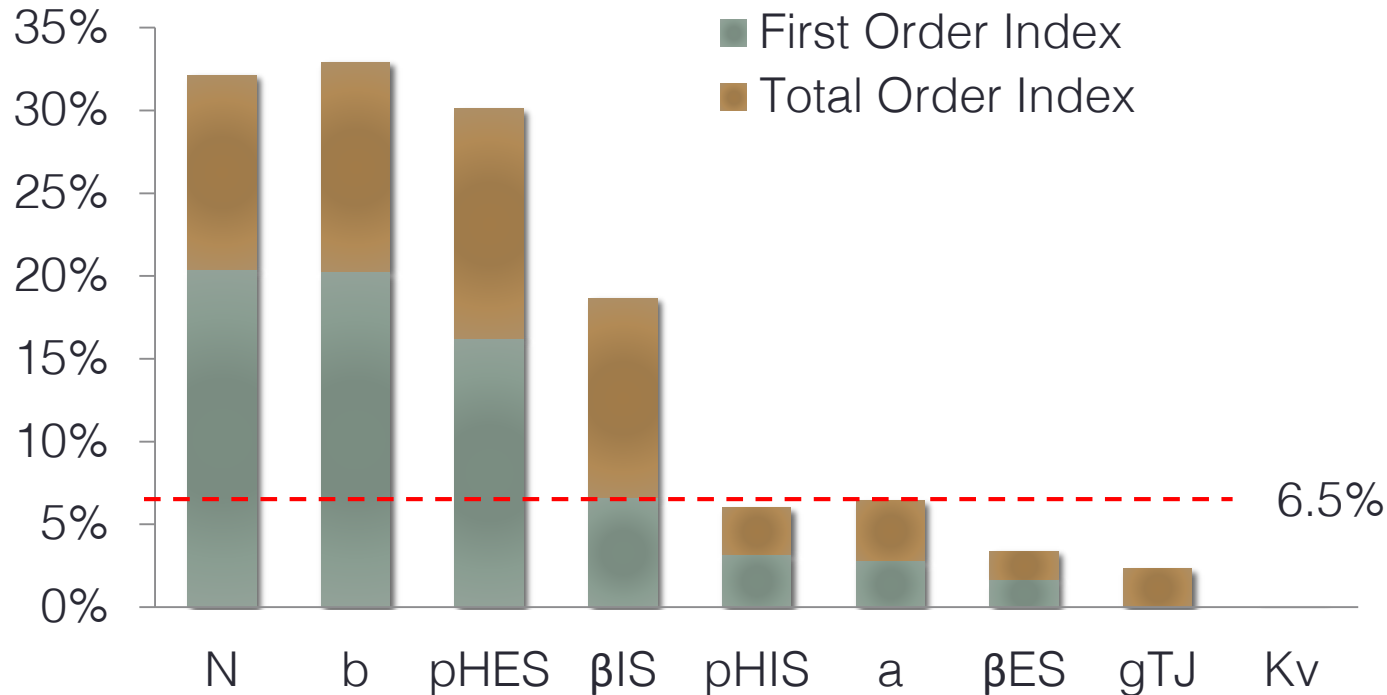
- Model's structure
- Probability density function assumed for each input factor
- Parameter value ranges

• Preliminary study

- Uniform distributions
- Largest possible value ranges for the input parameters



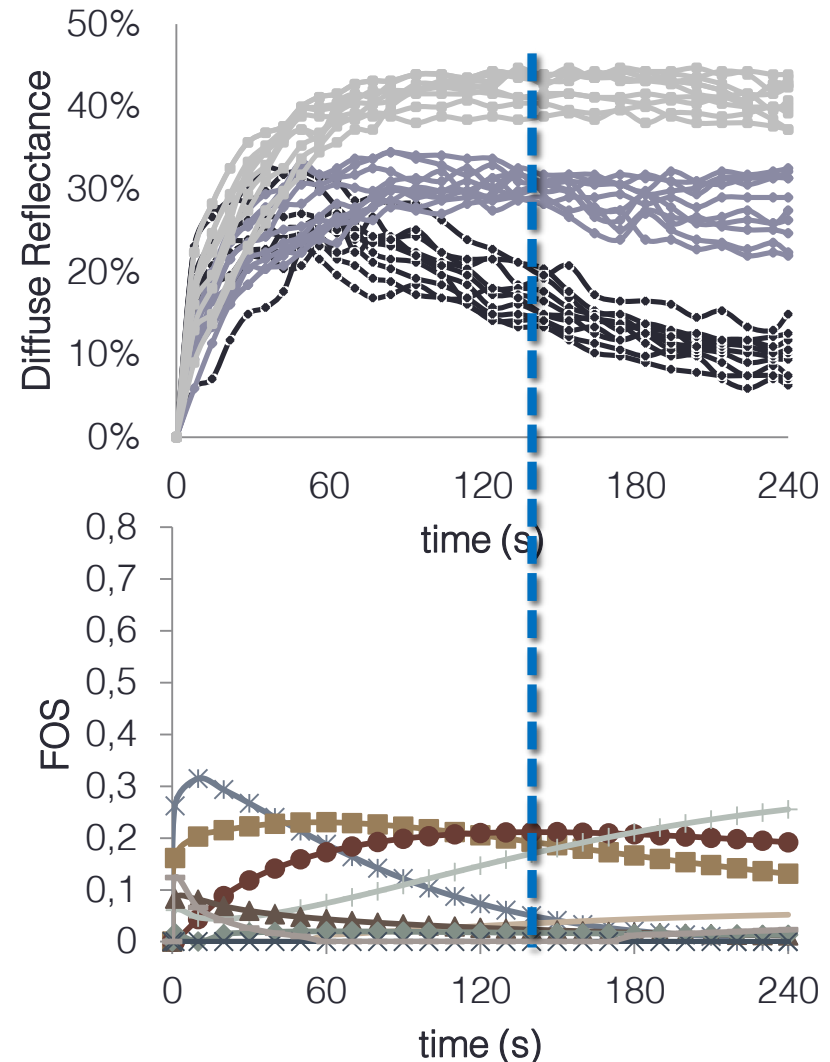
Parameter ranking



- **N**: histology grading parameter
- **b**: increases with neoplasia progression (Walker, et al., *Physiol. Meas.*, 2003)
- **pH_{ES}**: precursor of invasive cells (Gatenby, et. al., *Cancer Res.*, 2006)
- **β_{IS}** : cell's dominant suppressor of the acute increase in intracellular H⁺
- Total index of the rest of the parameters was less than 6.5% suggesting a negligible effect on the model's output

Correspondence with experimental data

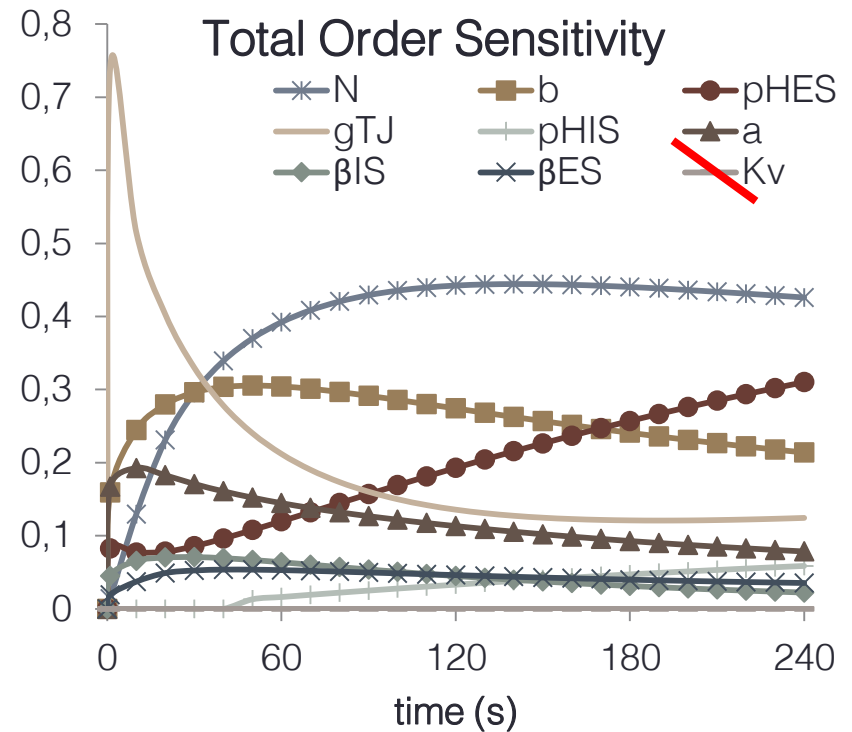
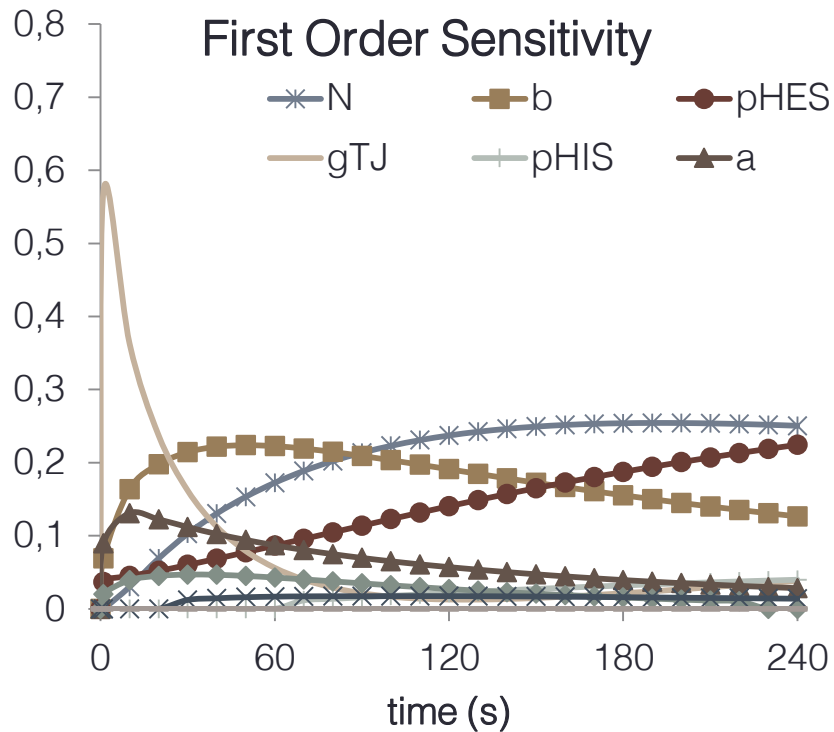
- Neoplasia grade is highly correlated with the number of dysplastic layers (N)
 - N can be assessed in a semi-quantitative manner from biopsy samples
- 30 experimental curves (biopsy confirmed)
 - 10 CIN I (low grade) and
 - 20 CIN II, III (high grade)
- At $t=142s$ where the importance of N maximizes the change of the median reflectance value is 1.25 times
- Suggests a correspondence between theoretical predictions and experimental data



Revisited global sensitivity analysis

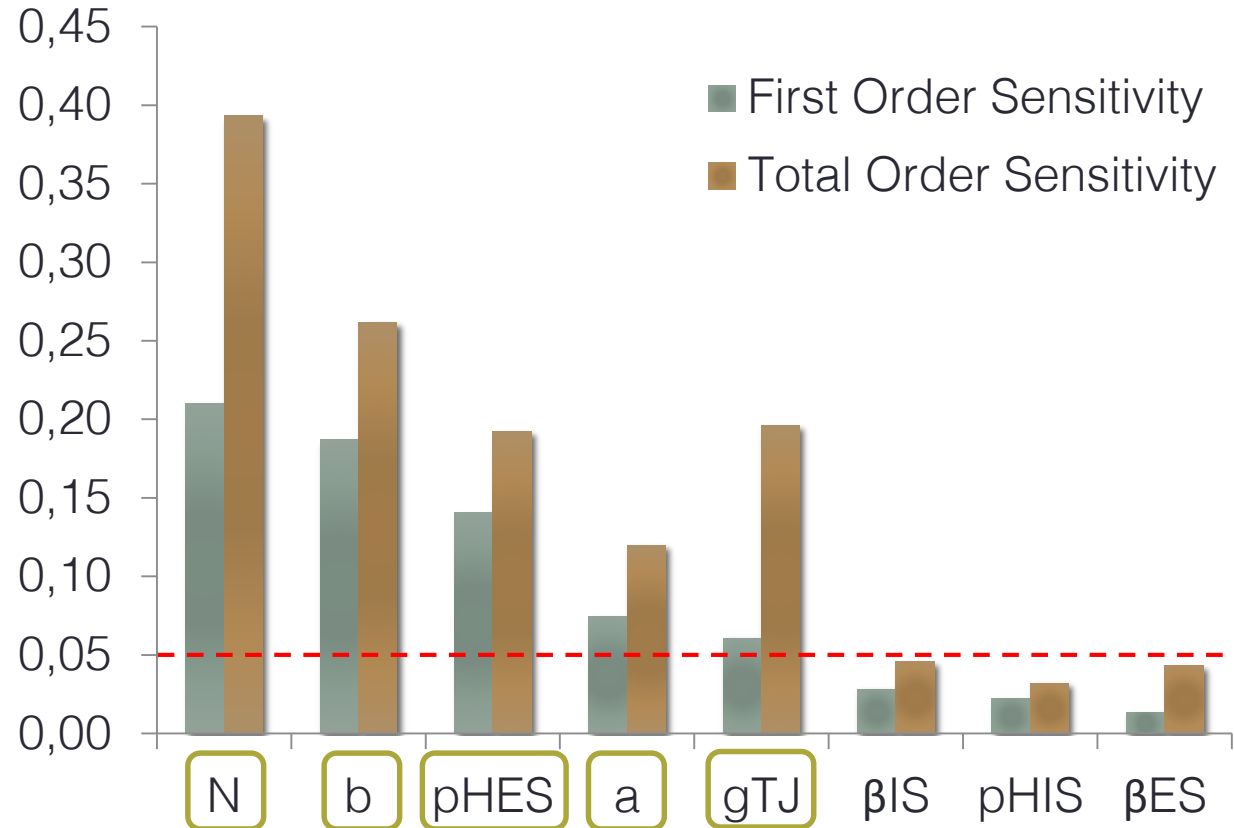
- Parameter distributions
 - Thorough literature study
 - Uniform: N , β_{ES} , β_{IS} , pH_{ES} , pH_{IS} , a
 - Triangular: b , K_V
 - Log-triangular: g_{TJ}

- Corrected parameter values
- Model update



Parameter ranking (revisited)

descending mean FOS index



The influence of the rest of the parameters was less than 5% suggesting a **negligible** effect on the model's output

Parameter collinearities

$$\mathbf{S}_D = \begin{bmatrix} S_{T_1|t_1} & \cdots & S_{T_k|t_1} \\ \vdots & \ddots & \vdots \\ S_{T_1|t_s} & \cdots & S_{T_k|t_s} \end{bmatrix}$$

Pearson's r



a	1	0,58	0,44	0.95 (1)	-0,73	-0,90	-0,93	0,87
b	0,58	1	0.96 (1)	0,76	0,12	-0,53	-0,51	0,12
β_{ES}	0,44	0.96 (1)	1	0,67	0,24	-0,44	-0,41	-0,03
β_{IS}	0.95 (1)	0,76	0,67	1	-0,55	-0,93	-0,93	0,68
N	-0,73	0,12	0,24	-0,55	1	0,72	0,77	-0,93
pH_{ES}	-0,90	-0,53	-0,44	-0,93	0,72	1	0.99 (1)	-0,73
pH_{IS}	-0,93	-0,51	-0,41	-0,93	0,77	0.99 (1)	1	-0,79
g_{TJ}	0,87	0,12	-0,03	0,68	-0,93	-0,73	-0,79	1
	a	b	β_{ES}	β_{IS}	N	pH_{ES}	pH_{IS}	g_{TJ}

Reduced set

1	0,60	-0,80	-0,87	0,9	a
0,60	1	-0,02	-0,66	0,19	b
-0,80	-0,02	1	0,68	-0,94	N
0,87	-0,66	0,68	1	-0,67	pH_{ES}
0,9	0,19	-0,94	-0,67	1	g_{TJ}
a	b	N	pH_{ES}	g_{TJ}	

Full set

1	1	1	1	1	1
0,95-1	0,9 - 0,94	0,7 - 0,89	0,4 - 0,69	0,1 - 0,39	0 - 0,09

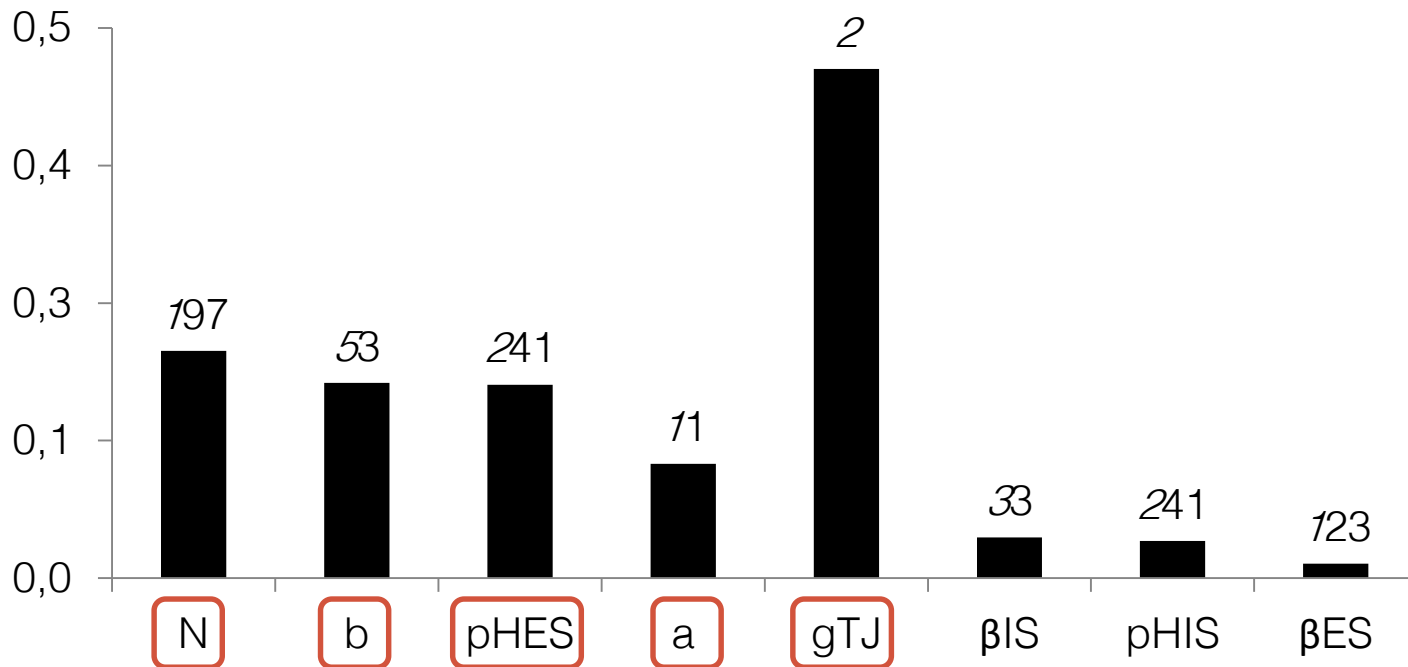
- Repeatedly remove one unidentifiable parameter each time ($r > 0.95$)
- Choose according to disease specific importance

Estimability Analysis

Parameter interdependencies

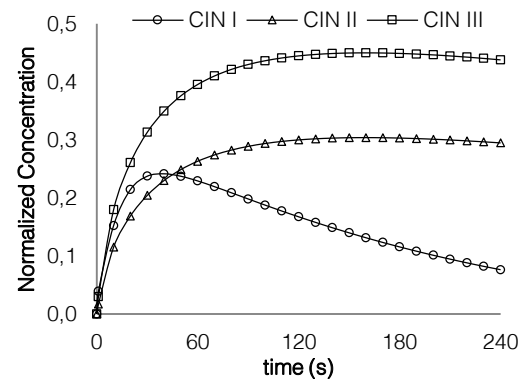
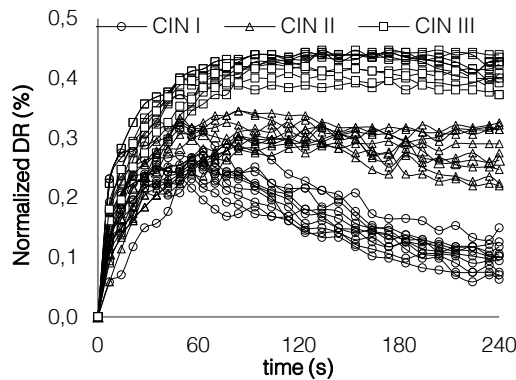
$$ER(t) = S_i(t) / \sum_{j=1}^k S_{T_j}(t)$$

- Similar to the FOS ranking
- high ranking of g_{TJ} : high FOS index at first time instances

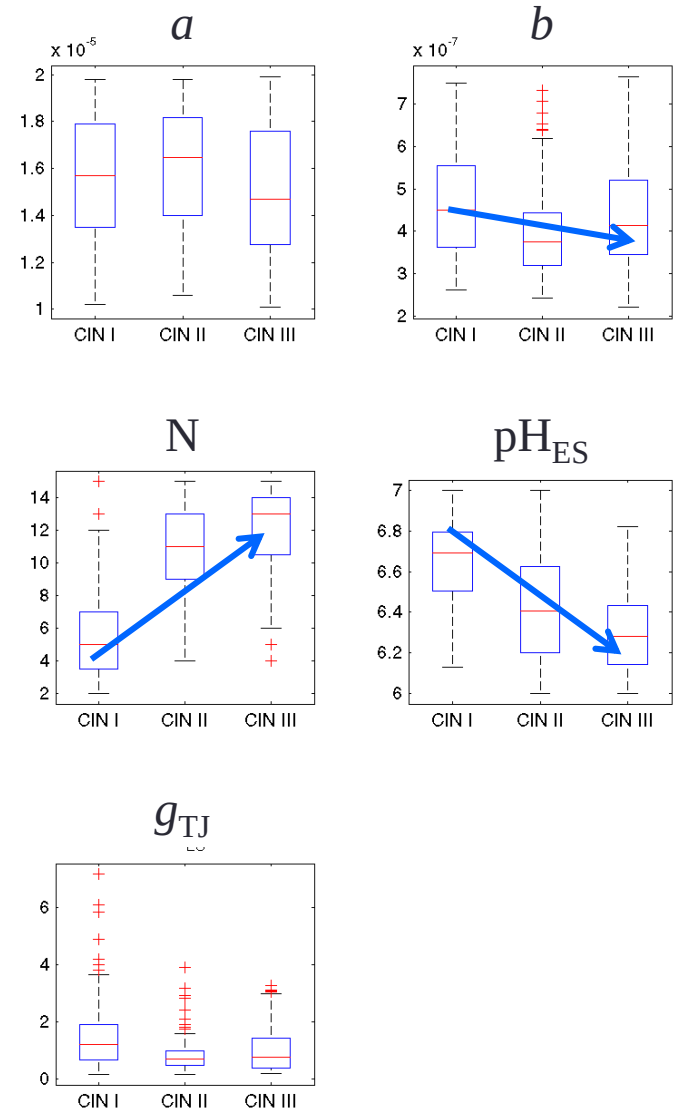


High level validation of the dimensionality reduction

- 30 NDR vs. time experimental curves
 - 10 CIN I (LG), 10 CIN II and 10 CIN II (HG)
- fitting by comparison with 20.000 normalized $[H^+]$ vs. time curves (GSA)
 - not unique set of parameter combinations
 - fit each experimental curve with ten, best fitting model curves ($R^2 > 93\%$)
 - assign 100 curves to each CIN class



This has shown for the first time that the solution of the inverse problem can be possible



Model restructuring (1)

- **dynamic range of b**
 - significant histology parameter
 - high overlapping of the estimated values
- **remodel parameter g_{TJ}**
 - high collinearity with N

Full set

N	1	0,25	0,55	-0,91	-0,56	0,79	0,51	-0,83
b	0,25	1	-0,44	0,13	0,65	-0,27	0,92	0,28
pH_{ES}	0,55	-0,44	1	-0,66	-0,77	0,92	-0,08	-0,67
g_{TJ}	-0,91	0,13	-0,66	1	0,84	-0,88	-0,17	0,99 (1)
β_{IS}	-0,56	0,65	-0,77	0,84	1	-0,84	0,37	0,91
pH_{IS}	0,79	-0,27	0,92	-0,88	-0,84	1	0,11	-0,87
β_{ES}	0,51	0,92	-0,08	-0,17	0,37	0,11	1	-0,01
a	-0,83	0,28	-0,67	0,99 (1)	0,91	-0,87	-0,01	1
	N	b	pH_{ES}	g_{TJ}	β_{IS}	pH_{IS}	β_{ES}	a

before restructuring

a	1	0,58	0,44	0,95 (1)	-0,73	-0,90	-0,93	0,87
b	0,58	1	0,96 (1)	0,76	0,12	-0,53	-0,51	0,12
β_{ES}	0,44	0,96 (1)	1	0,67	0,24	-0,44	-0,41	-0,03
β_{IS}	0,95 (1)	0,76	0,67	1	-0,55	-0,93	-0,93	0,68
N	-0,73	0,12	0,24	-0,55	1	0,72	0,77	-0,93
pH_{ES}	-0,90	-0,53	-0,44	-0,93	0,72	1	0,99 (1)	-0,73
pH_{IS}	-0,93	-0,51	-0,41	-0,93	0,77	0,99 (1)	1	-0,79
g_{TJ}	0,87	0,12	-0,03	0,68	-0,93	-0,73	-0,79	1
	a	b	β_{ES}	β_{IS}	N	pH_{ES}	pH_{IS}	g_{TJ}

1	0,60	-0,80	-0,87	0,9	a
0,60	1	-0,02	-0,66	0,19	b
-0,80	-0,02	1	0,68	-0,94	N
0,87	-0,66	0,68	1	-0,67	pH_{ES}
0,9	0,19	-0,94	-0,67	1	g_{TJ}
a	b	N	pH_{ES}	g_{TJ}	

Reduced set

1	-0,24	-0,40	-0,83	N
-0,24	1	-0,49	0,72	b
-0,40	-0,49	1	0,09	pH_{ES}
-0,83	0,72	0,09	1	g_{TJ}
N	b	pH_{ES}	g_{TJ}	

Model restructuring (2)

- **alleviate parameter a**
 - within the highest ranked ones
 - lowest ranked
 - smallest ER
 - high collinearities with the rest of the parameters (negative effect on the identifiability of these parameters)
 - lowest correlation with neoplasia development according to model assumptions
-

Result 3: Critical, neoplasia-related parameters

Systematic parameter reduction

- K_V : null TOS function
- β_{IS} , β_{ES} , pH_{IS} : close to unity correlation coefficient + low ER + low FOS
- a : high collinearity with the highest ranked parameters

key determinants of the measurable/modeled dynamic optical characteristics

- N , b are the key parameters onto which routine histological grading of biopsies is based
- pH_{ES} is strongly linked with the ability of tumor cells to form invasive cancers
- g_{TJ} represents the tight junction functional changes due to malfunction at precancers

Concurrent estimation and for every spatial point of the tissue is possible through optical measurements.

Ideally, diagnosis and prediction can be performed at the same consultation and non-invasively

THESIS RESULTS & CONTRIBUTIONS

Conceptualization

Mathematical
Implementation

Sensitivity
Analysis

Solve the
inverse

Parameter mapping

4. SOLUTION OF THE INVERSE PROBLEM

Problem statement

In silico experimental setup

Results

Result 4: Solution of the inverse problem

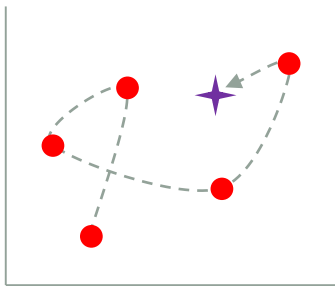
- **We quantitated the overall quality of the solutions to the inverse problem**
 - Aggregate error < 5%
- **Estimation of the four most important biological parameters, is possible with highly accuracy and reproducibility using DE or CRSwCH methods**
 - Aggregate error ~1%

Relevant publications

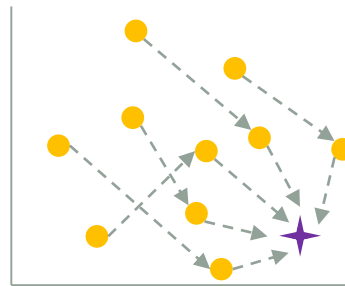
1. Papoutsoglou G., Stamatiadou M., Stavrakakis G., Balas C., *"In vivo Estimation of Functional and Structural Characteristics in Epithelial Neoplasia"*, OSA Optical Molecular Probes, Imaging and Drug Delivery (OMP), Monterey, California, USA, April 4, 2011
 2. G. Papoutsoglou, M. Stamatiadou, and C. Balas, *"In silico Modeling and Global Optimization of Dynamic Bio-optical Processes for Probing, in vivo, Biological Features of Neoplasia,"* IEEE iCBEB, Macau, China, 2012
-

Employed global optimizers

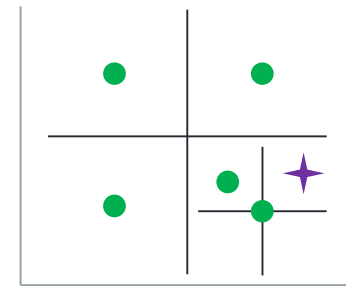
- **no guarantee of optimality**
 1. find sets of solutions by several dissimilar methods
 2. decide the degree of convergence that is actually achieved
- **Deterministic**
 - gblSolve
- **Stochastic**
 - Controlled Random Search with Competing Heuristics (CRSwCH)
 - Differential Evolution (DE)
 - Shuffled Complex Evolution (SCE)
 - Particle Swarm Optimization (PSO)
 - ThermoDynamically Adaptive Simulated Annealing (tdASA)
 - Stochastic Ranking Evolutionary Strategy (SRES)
 - Mixed-Integer Dynamic Ant Colony Optimization (MIDACO)



Point to Point

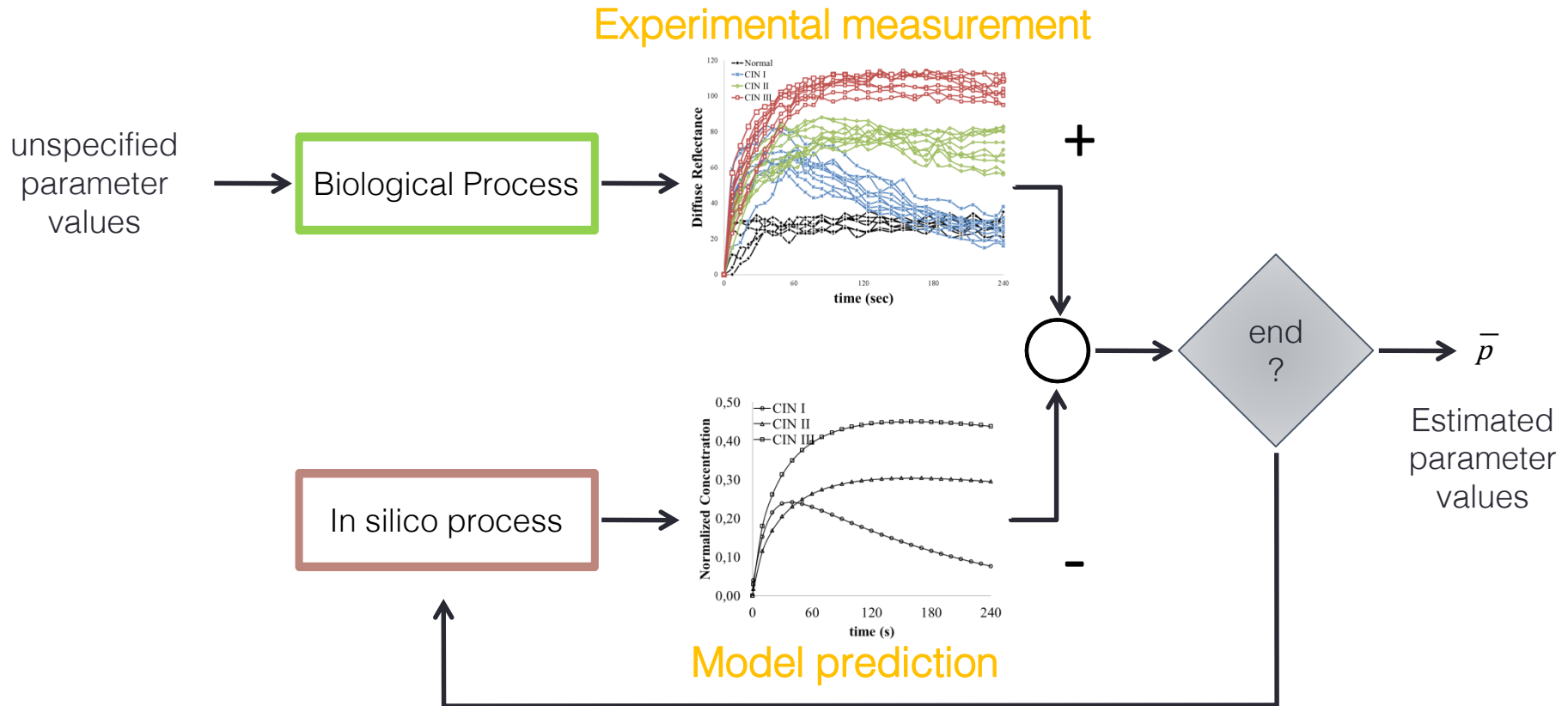


Population based



Bound division

Derivative-free parameter estimation



Problem statement

$$\text{minimize} \quad J = \left\| y^{\text{exp}}(\mathbf{p}, t) - y^{\text{M}}(\bar{\mathbf{p}}, t) \right\|,$$

$$\text{subject to} \quad f\left(\frac{d\mathbf{x}}{dt}, \mathbf{x}, \bar{\mathbf{p}}, \mathbf{u}, t\right) = 0 \quad \longrightarrow \quad \text{system dynamics}$$

$$\mathbf{x}(t_0) = \mathbf{x}_0 \quad \longrightarrow \quad \text{initial conditions}$$

$$t \in [0, 240] \quad \longrightarrow \quad \text{time}$$

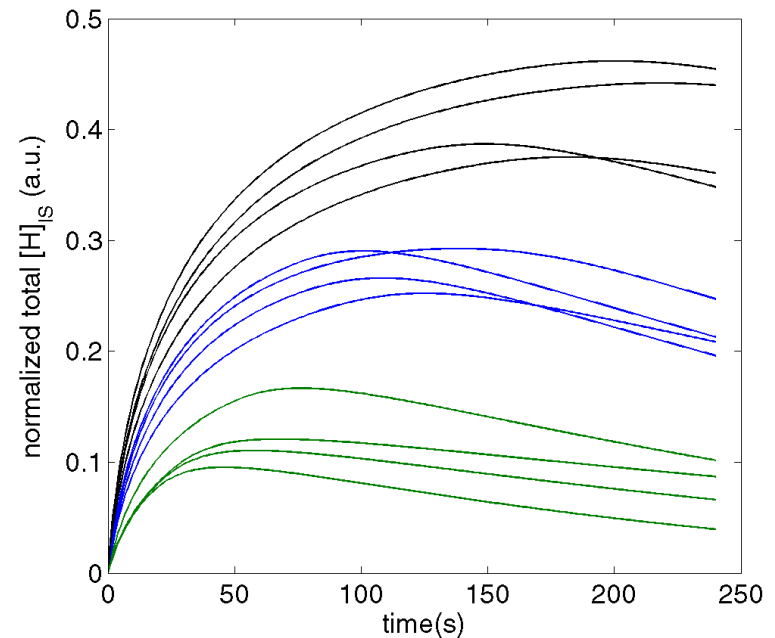
$$\mathbf{p}_L \leq \bar{\mathbf{p}} \leq \mathbf{p}_U \quad \longrightarrow \quad \text{parameter space}$$

$$\mathbf{u} = u_0 \quad \longrightarrow \quad \text{input}$$

- **non linear**
- **mixed-integer**
- **differential-algebraic constraints**
- **NP-complete**

In silico experimental setup

- **Test problem: 30 pseudo-experimental (PEX) curves.**
 - 10 manually selected,
 - represent all the clinical stages of neoplasia
 - 10 by step-wise sampling
 - 10 randomly selected
- **Two PEX data ensembles**
 - full set
 - reduced set
- **Exact results devoid of measurement noise**



Let the model be accurate and complete, then the validation of the solvability of the inverse problem is possible if repeatable convergence to unique solutions is achieved.

Performance estimation formulas

Each PEX curve is fitted 30 times ~9 hours (max)

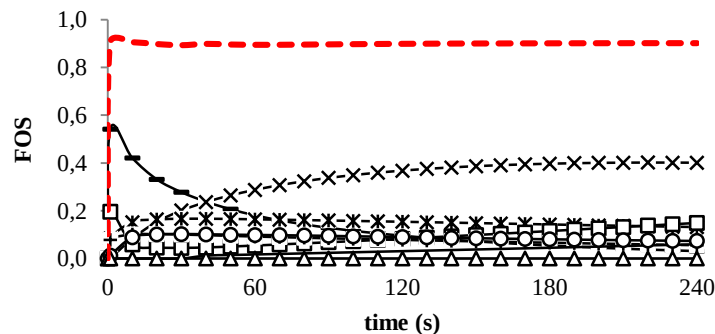
Parameter estimation accuracy

$$NRMSD(p)_k^{PE} = \frac{RMSD(p)_k^{PE}}{(p_{\max} - p_{\min})} = \frac{\sqrt{\sum_{i=1}^{30} (p_{i,k}^{PE} - \hat{p}_k^{PE})^2}}{30 \cdot (p_{\max} - p_{\min})}$$

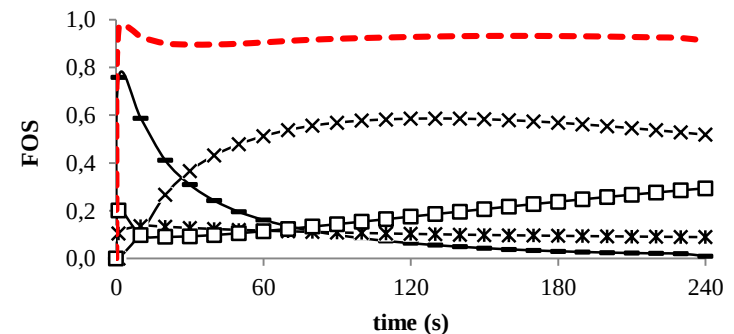
Aggregate algorithmic accuracy per PEX

$$error_{al}^{PEX} = \sum_{i=1}^k \left\{ w g_i \times NRMSD(p_i)_{al}^{PEX} \right\}, \quad w g_i \cong \sum_{i=1}^{240} \frac{FOS(p_i)}{240}$$

8 parameters

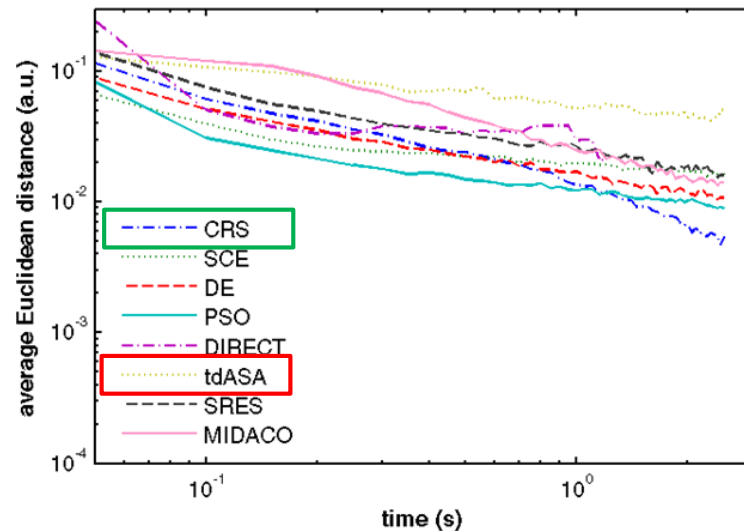


4 parameters

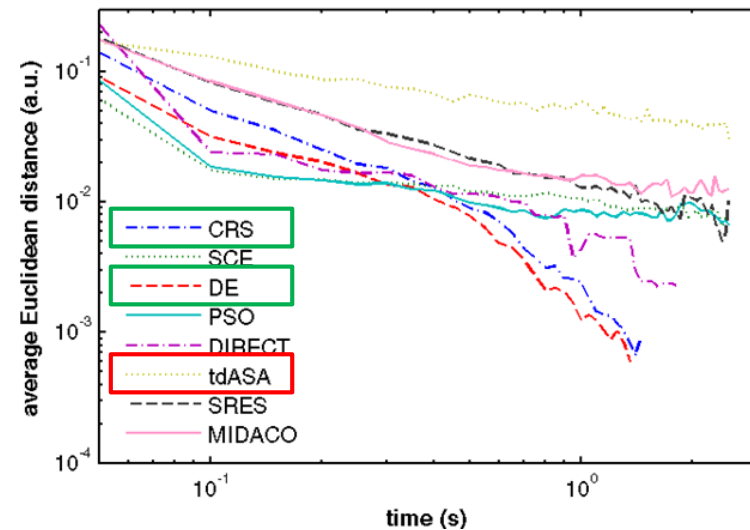


Convergence efficiency

8 parameters



4 parameters

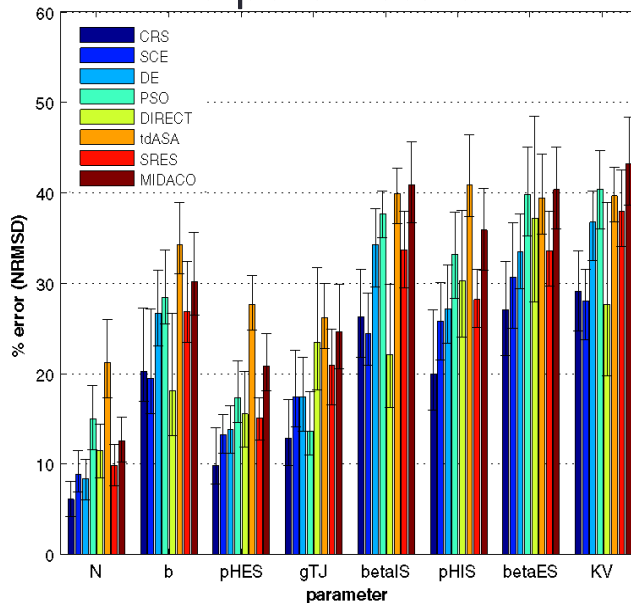


- Average Euclidean distance over all repetitive runs and all PEX data (every 3 seconds)
- **Full parameter case:** algorithms terminate most probably due to entrapment to locally optimum solutions
- **Reduced parameter case:** algorithms terminate most probably due to curve convergence

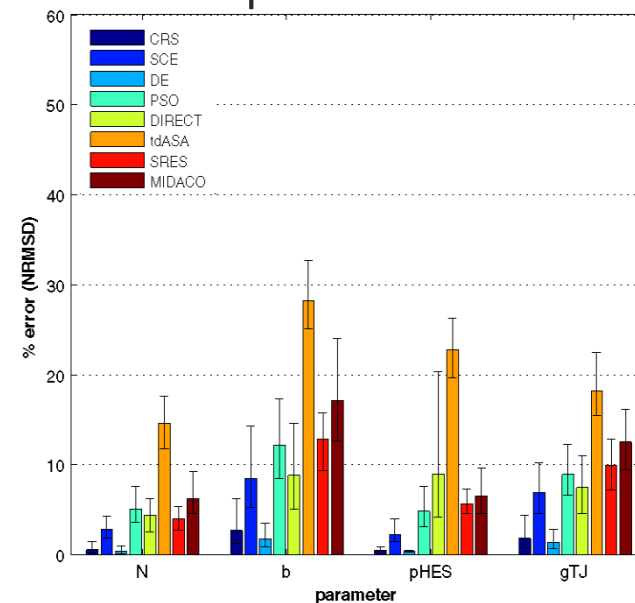
Efficient : CRSwCH, SCE, DE // **Inefficient:** tdASA, MIDACO, SRES

Parameter estimation results

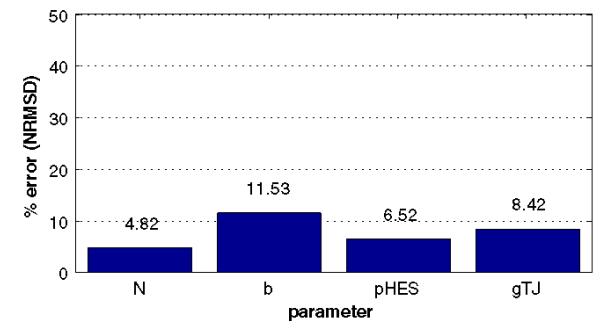
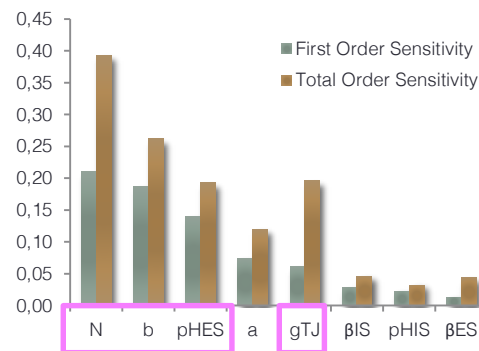
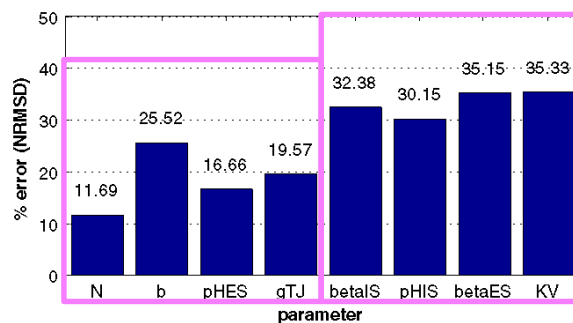
8 parameters



4 parameters



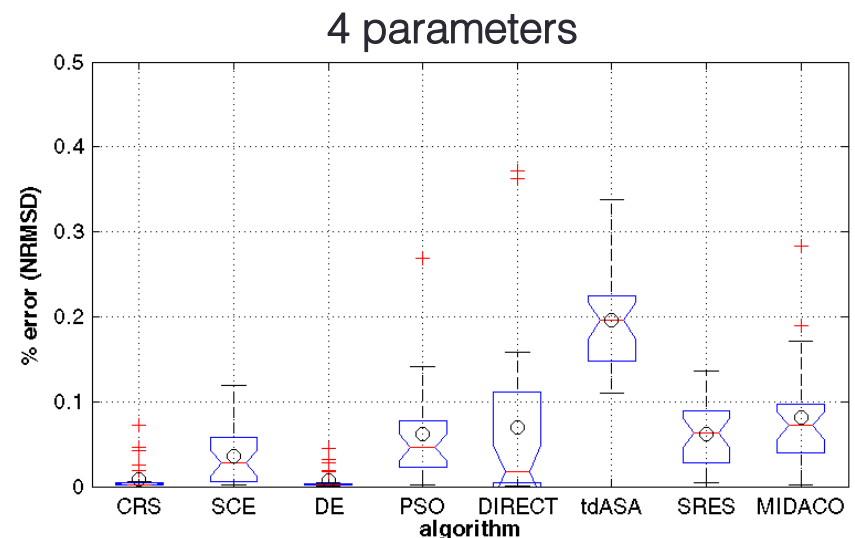
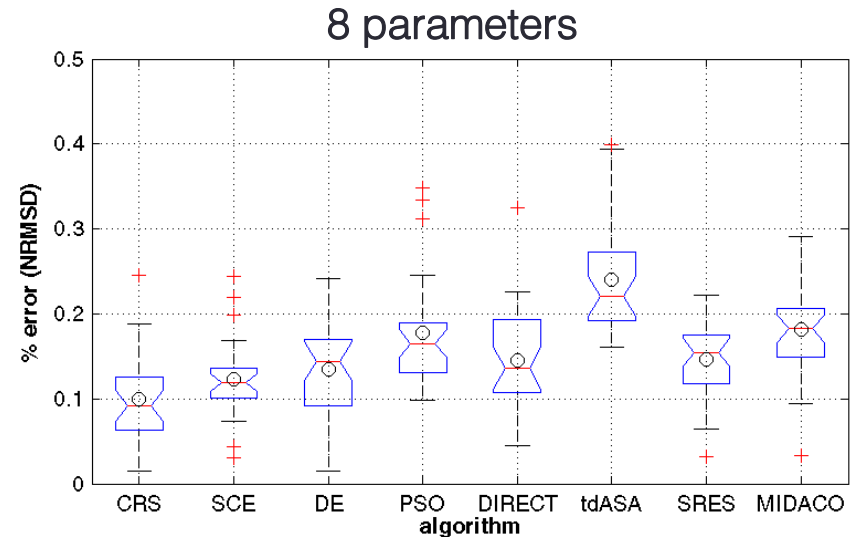
Aggregate estimation error (mean)



GSA validation

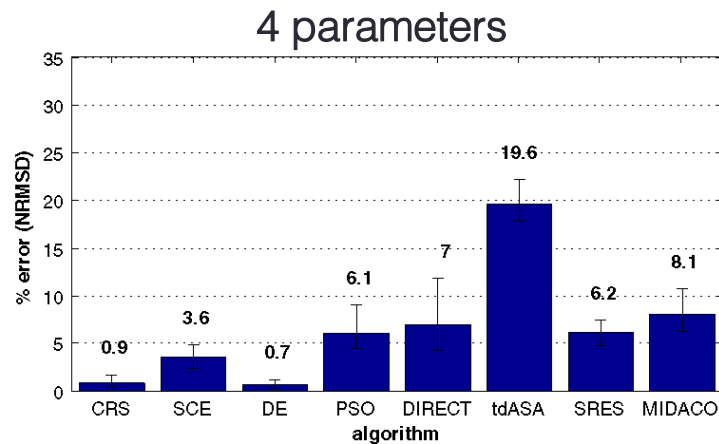
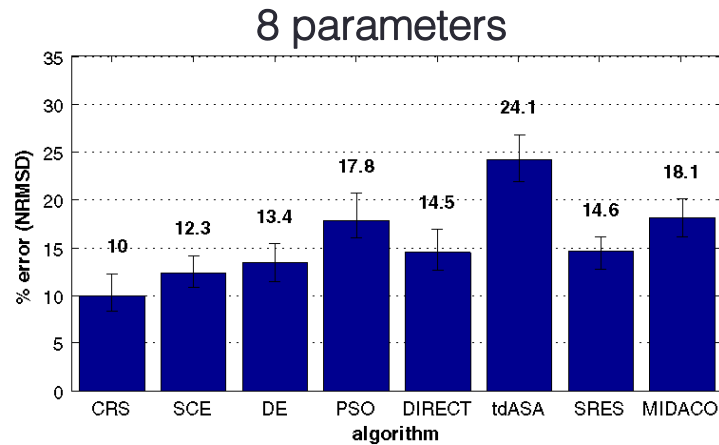
Accuracy of the parameter estimations

- **high variance + outliers**
 - some algorithms have trouble to repeatedly reach a satisfactory low parameter estimation error
 - some PEX signals lead to more difficult optimization tasks
 - robustness: mean vs. median
- **Full parameter case**
 - many locally optimal solutions
 - fixing unimportant parameters is needed (GSA)
- **Reduced parameter case**
 - Low accuracy due to insufficient optimization time



Algorithm performance

Student's *t*-test



$$error_{al}^{PEX} = \sum_{i=1}^k \left\{ w g_i \times NRMSE(p_i)_{al}^{PEX} \right\},$$

Algorithm	$\mu_{al} \leq 5\%$		$\mu_{al} \leq 8.5\%$	
	P-value	Hypothesis	P-value	Hypothesis
CRSwh	$2,8 \cdot 10^{-42}$	accepted	$4,7 \cdot 10^{-48}$	accepted
SCE	0,02	accepted	$1,3 \cdot 10^{-08}$	accepted
DE	$5,7 \cdot 10^{-43}$	accepted	$1,0 \cdot 10^{-48}$	accepted
PSO	0,69	rejected	0,0002	accepted
DIRECT	0,46	rejected	0,0007	accepted
tdASA	1	rejected	1	rejected
SRES	0,95	rejected	0,0011	accepted
MIDACO	0,98	rejected	0,046	accepted

Holm-Sidak multiple comparison test

<i>i</i>	Test	P-value	<i>a/i</i>	Hypothesis
7	DE – tdASA	0.0000	0.0073	rejected
6	DE – MIDACO	0.0000	0.0085	rejected
5	DE – DIRECT	0.0000	0.0102	rejected
4	DE – SRES	0.0001	0.0127	rejected
3	DE – PSO	0.0001	0.0170	rejected
2	DE – SCE	0.0364	0.0253	fail to reject
1	DE – CRSwh	0.8641	-	accepted

Result 4: Solution of the inverse problem

- The inverse problem is solvable using DE or CRSwCH methods
 - Predicted value deviations ~1%
 - high degree of convergence
 - almost unique set of parameters' for a given experimental curve
 - Statistical tests: it is unlikely for the predictions to have occurred by chance
 - The method is capable of estimating, with adequate accuracy, both structural and functional characteristics associated with the growth of epithelial neoplasia.
 - Global optimization, computational biology and DCE-OI approaches have been employed together for the **first time**
-

THESIS RESULTS & CONTRIBUTIONS

Conceptualization

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inverse

Parameter mapping

5. IN VIVO MAPPING OF NEOPLASIA RELATED TISSUE PARAMETERS

Clinical data

Correlation of predictions with progresses of neoplasia

Parameter mapping

Interpretations

Result 5: Mapping predictions

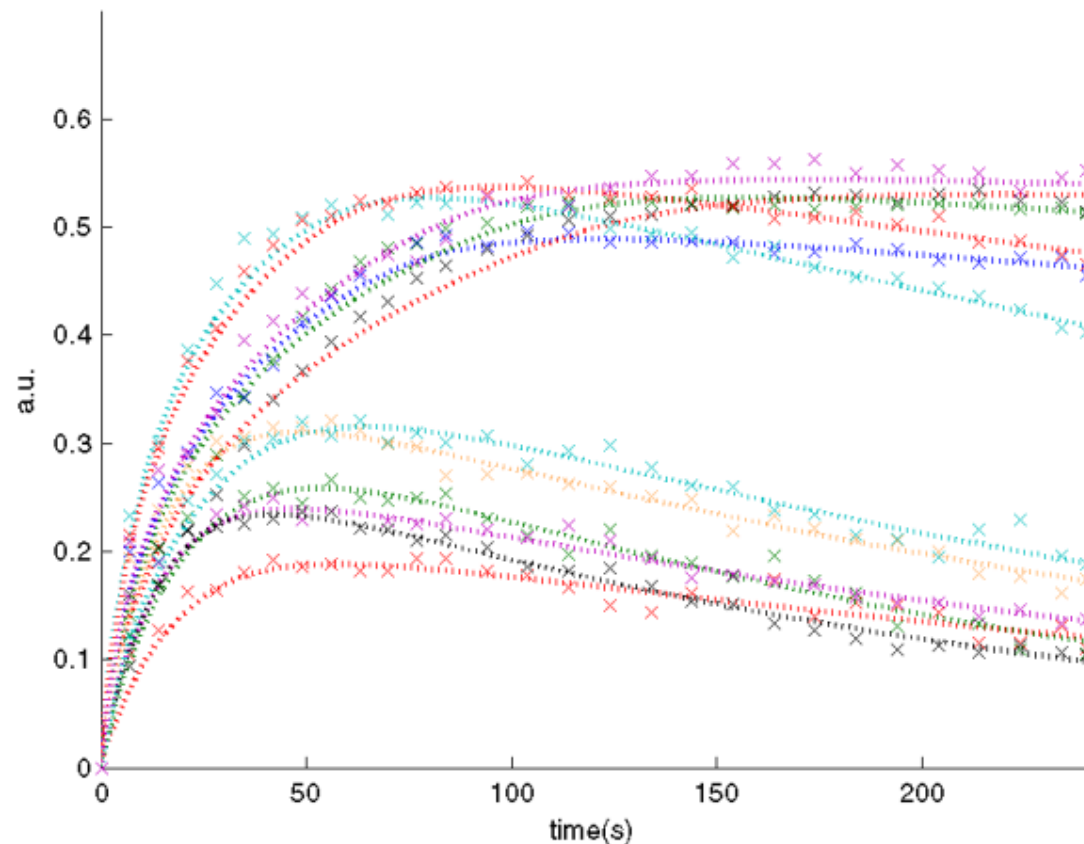
- Concurrent estimation of the key biological parameters from *in vivo* measurements and for every spatial point is possible
- Our model is largely predictive
 - no contradiction between our results and literature
- Provide new insights in study of epithelial neoplasia
- We present a novel non invasive diagnostic method that contributes to cancer prevention.

Relevant publications

G. Papoutsoglou, Theodoros-Marios Giakoumakis, and C. Balas, “Dynamic contrast enhanced optical imaging of cervix, *in vivo*: A paradigm for mapping neoplasia-related parameters.,” in Conference proceedings : Annual International Conference of the IEEE Engineering in Medicine and Biology Society. Conference, Osaka, Japan, 2013, vol. 2013, pp. 3479–82

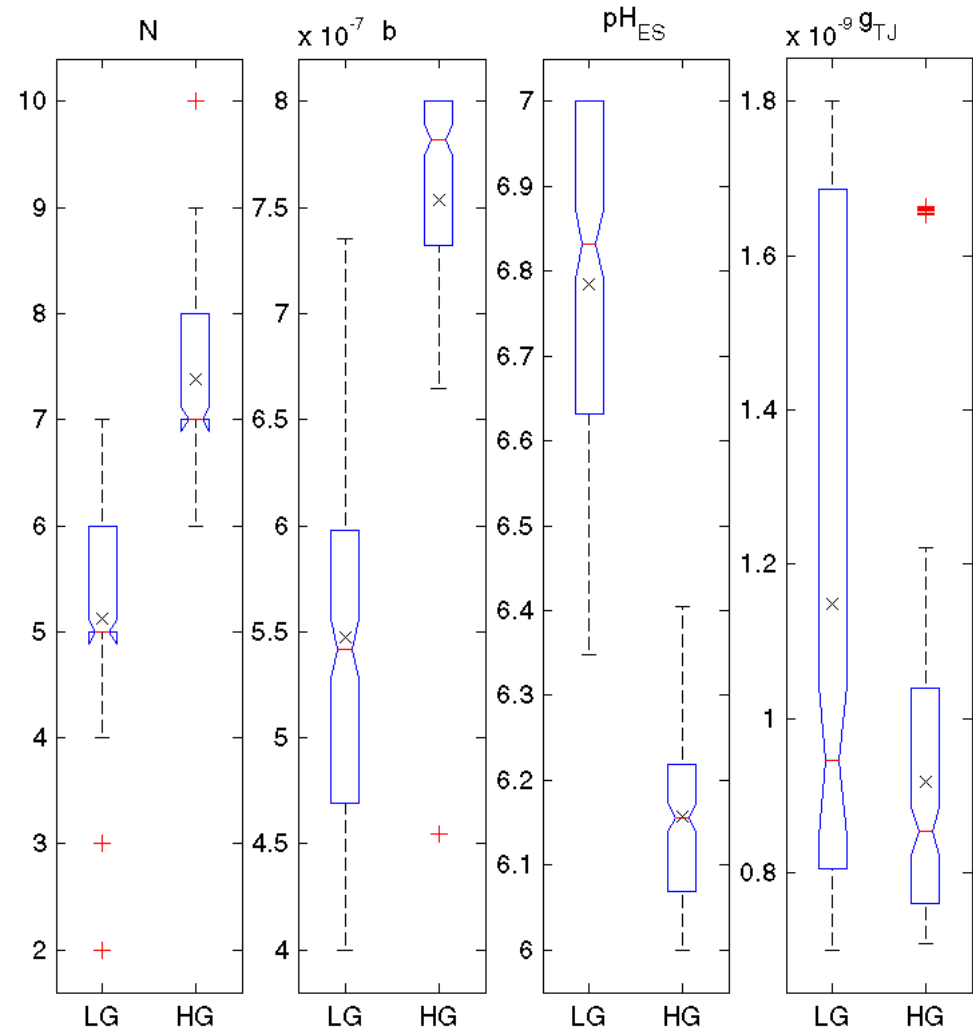
Correlation of predictions with neoplasia growth (1)

- Collect representative DR curves from each biopsy point (40)
- Fit using the best GO method
 - Normalize
 - Data smoothing

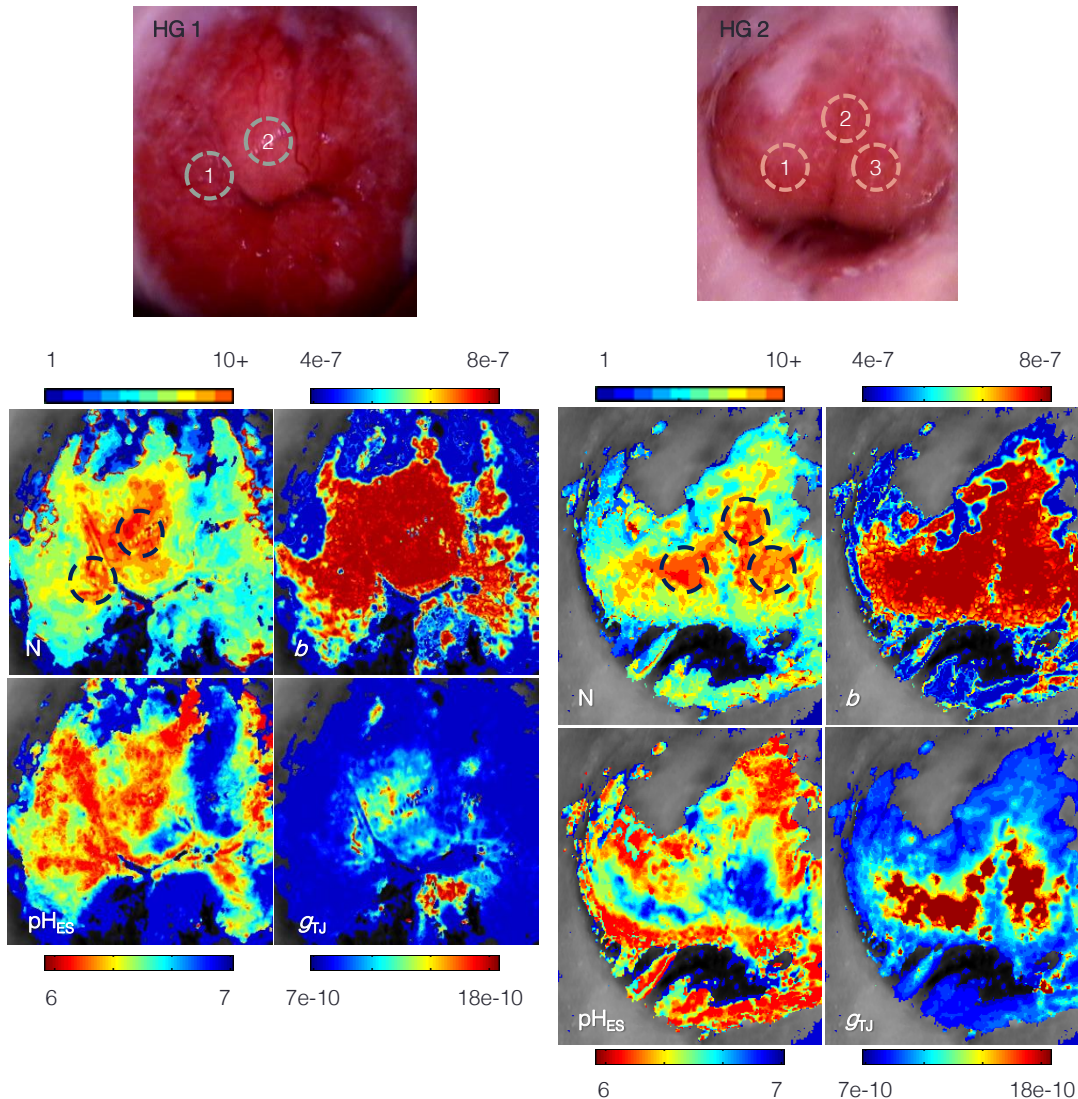


Correlation of predictions with neoplasia growth (2)

- **N: high correlation**
 - neoplasia progression can be, in principle, predicted from the estimated values of the structural parameters such as the dysplastic cell packing
- **b: high correlation**
 - consistent with literature
 - results robustness
- **pH_{ES}: high correlation**
 - acid-mediated tumor invasion model
- **g_{TJ}: no significant correlation**
 - consistent with incoherent literature reports



High grade



N

- high accumulation in HG areas
- size of lesion
 - additional criterion in colposcopy
- lesion within lesion
 - discriminate within the group of HG

b

- delineates the TZ
- atypical vasculature
 - mosaic pattern
 - punctuation
- diffusion areas

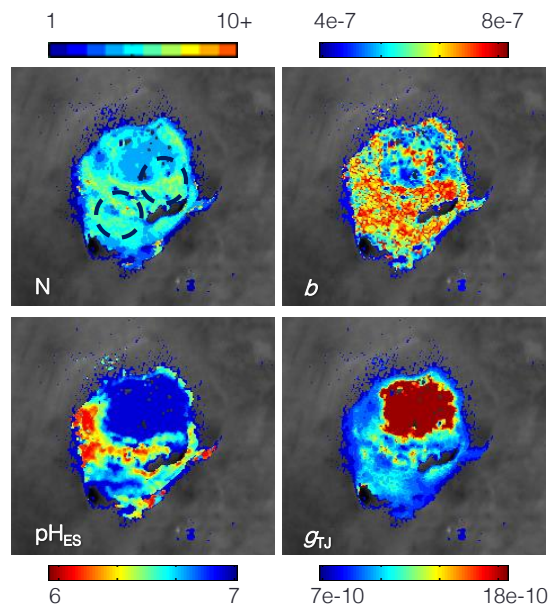
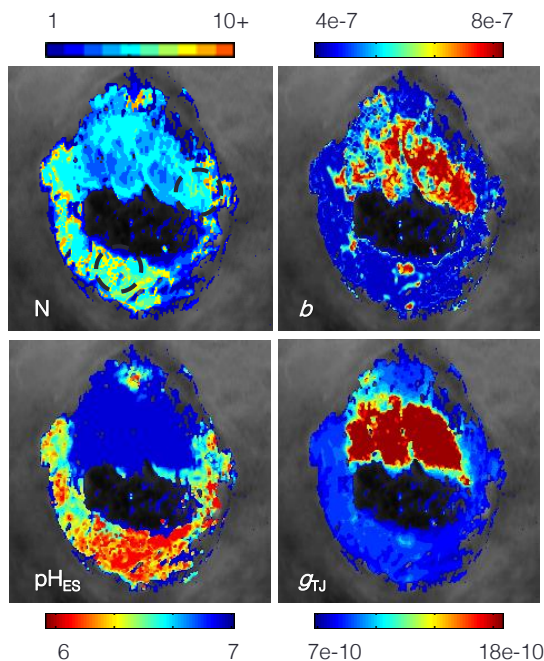
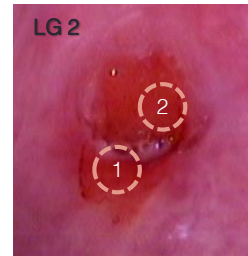
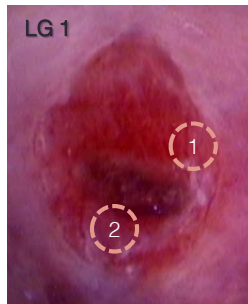
pH_{ES}

- cancer spreading
- invasion areas

g_{TJ}

- permittivity of tissue
- discriminate CIN II from III

Low grade



N

- low cell packing
- indistinct lesion
 - no sharp edges
 - no large tissue patches

b

- large ES exactly where biopsy is taken
 - method's sensitivity
- not excessive atypical vasculature
 - several color codes (metaplasia or LG)
- high values
 - pathogens
 - natural secretion or absorption

pH_{ES}

- exaggerate low values
 - columnar epithelium
 - slow onset of AW
- cancer spreading

g_{TJ}

- explains low pH_{ES}

Result 5: Mapping predictions

- **Our predictions conforms to the biology of the cervix during the progression of neoplasia from LG to HG**
 - our model is largely, predictive
 - **Concurrently estimated the key biological parameters from *in vivo* measurements and for every spatial point**
 - Our predictions for the number of dysplastic layers, which is the golden standard for histology classification, have been in total agreement with the doctors' assessments
 - Pseudocolor mappings are compatible with literature findings for both HG and LG neoplastic epithelia
 - Extract diagnostic information
 - **We presented a novel non invasive diagnostic method that contributes to cancer prevention**
 - New insights in study of epithelial neoplasia
 - Can be exploited as a new optical biopsy technique
 - Detect the biodistribution and pharmacokinetic properties of contrast agents
 - Simply improve imaging of targeted contrast agents
-

CONCLUSIONS

Summary

Ongoing research

Forward looking and further developments

What we answered

- **Bio-Optical study**
 - Elucidated the origins of the dynamic optical phenomenon
- **Mathematical framework**
 - Developed a coherent model
 - Preliminary validation with experimental data
- **Sensitivity analysis**
 - Systematic reduction of model's complexity
 - most critical parameters with profound correlation with disease progression
- **Inverse problem solution**
 - In principle solvable
 - DE and CRSwCH are the most suitable algorithms
- **Parameter mapping**
 - Interpreted and correlated predictions and experimental results with literature and clinical practice
 - Added diagnostic information previously unattainable

Bio-Optical
study

Mathematical
Framework

Sensitivity
Analysis

Solve the
inverse

Parameter
mapping

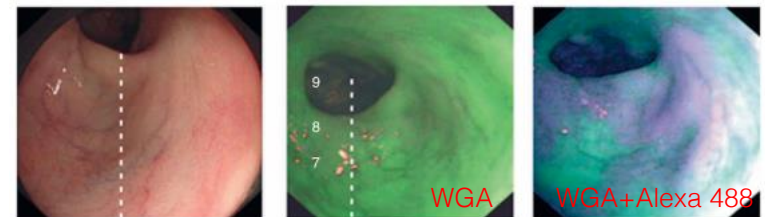
Our novel methodology holds the promise to become the next paradigm shift in cancer screening

Ongoing research

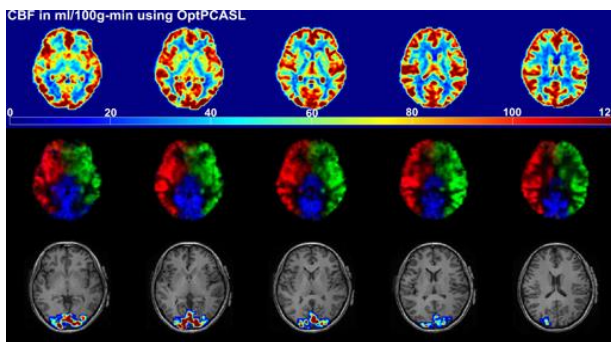
- **Improvement of time complexity**
 - Lookup table
 - Create an approximate, analytic model
 - HDRM
 - Test combinations of local and global algorithms
 - DE + gblSolve
 - Kriging + gblSolve
 - Step-wise fitting using the estimability ratios
-

Forward looking and further developments

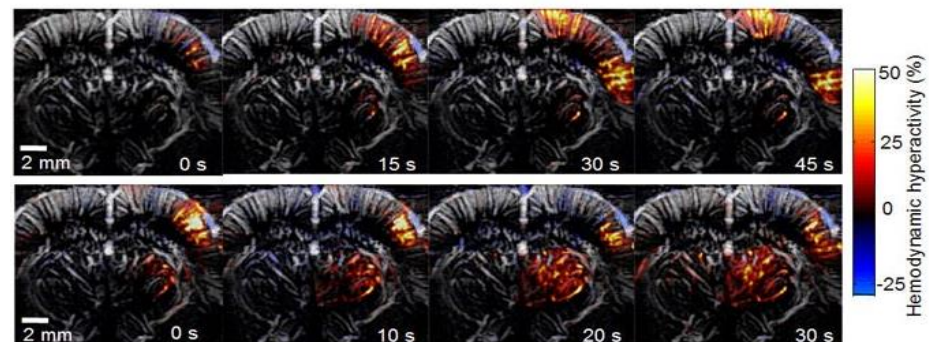
- **Application to other markers and tissues (optical molecular imaging)**
 - Fluorescent dyes (ex vivo, in vitro)
 - Non toxic markers (in vivo)
 - Oral cavity, skin, larynx, Barrett's esophagus, lymphatic nodes, etc.
- **Integration with other imaging modalities**
 - fMRI
 - functional Ultrasound
 - Fluorescent imaging
 - etc.



Bird-Lieberman, et al., *Nat. Med.*, 2012



<http://fmri.ucsd.edu/>



<http://medicalphysicsweb.org>

Possible innovative derivative product

Create a computational all-in-one suite that simulates pharmacodynamic/kinetic phenomena

Publications

Journal

1. Papoutsoglou G. and Balas C., "Estimation of Neoplasia-Related Biological Parameters through Modeling and Sensitivity Analysis of Optical Molecular Imaging Data", IEEE Transactions on Biomedical Engineering, Vol. 60, No. 5, pp. 1241-1249, 2013
2. ... (Journal of Biomedical Optics)

Conference

1. Papoutsoglou G., Giakoumakis T.M. and Balas C., "Dynamic Contrast Enhanced Optical Imaging of Cervix, in vivo: A Paradigm for Mapping Neoplasia-Related Parameters," to be presented at the 35th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC'13), 3-7 July, Osaka, Japan, 2013
 2. Papoutsoglou G., Stamatiadou M., and Balas C., "In silico modeling and global optimization of dynamic bio-optical processes for probing, in vivo, biological parameters of neoplasia", International Conference on Biomedical Engineering and Biotechnology (iCBEB), 28-30 May, Macau, China, 2012
 3. Papoutsoglou G., Anastasopoulou A., Stavrakakis G., Scouter P., Balas C., "In Vivo Dynamic Imaging, in Silico Modeling and Global Sensitivity Analysis for the Study and the Diagnosis of Epithelial Neoplasia," 33rd Annual International IEEE EMBS Conference, August 30 - September 3, Boston Marriott Copley Place, Boston, MA, USA, 2011
 4. Balas C., Papoutsoglou G., Diakomanolis E., Haidopoulos D. and Soutter W. P., "Quantitative Assessment of the AW phenomenon and determination of its biophysical origins as a means for in vivo assessing CIN-related micro-structural and functional changes," Journal of Lower Genital Tract Disease, vol. 14, pp. 264-269, ASCCP 2010 BIENNIAL MEETING, 24-27 March, Green Valley Ranch Resort, Las Vegas, NV, USA, 2010
 5. Balas C., Papoutsoglou G., Loukas C., Skiadas Y., Pappas C., Haidopoulos D., Diakomanolis E., Soutter W.P., "In vivo assessment of microstructural and functional alterations in cervical neoplasia", in the "Clinical and Biomedical Spectroscopy" conference, part of the OSA/SPIE European Conferences on Biomedical Optics, 14-18 June, Munich, Germany, 2009
 6. Balas C., Papoutsoglou G., Potirakis A., "In Vivo Molecular Imaging of Cervical Neoplasia Using Acetic Acid as Biomarker," IEEE Journal Of Selected Topics In Quantum Electronics, Vol. 14, No. 1, January/February, 2008
-

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Με τη συγχρηματοδότηση της Ελλάδας και της Ευρωπαϊκής Ένωσης



Thank you !!!

APPENDIX

Previous interpretations of the optical effect

- **occurs in**

- the nucleus of the cell: coagulation/precipitation of nucleoproteins
 - Maclean A., Lower Genital Tract Neoplasia, 2003
- cytoplasm: partial denaturation and possible polymerization of cytokeratins
 - S. Yamada, et al., Mol. Biol. Cell, 2002

- **occurs from**

- weak acids
 - reversible and lasts < 4min
 - sodium acetate and dicarboxylic acids such as lactic acid are not producing the effect
-

Maintaining the consistency of the results

- **Optimal tuning of intrinsic algorithm parameters**
 - Grid search
 - Literature
 - **Algorithm surgery**
 - parallel coding (7-cores, MatlabTM's matlabpool() function)
 - integer value by truncation
 - **Rules of fair comparison**
 - upper and lower bounds for the parameter values
 - common termination criteria
 - time or search effort: 2.5 minutes
 - curve convergence threshold (euclidean distance $< 10^{-3}$)
 - Population degenerates (geometric range $< 10^{-3}$)
 - computation power
 - CPU: i7 2,66GHz, RAM: 8GB,
 - MatlabTM 2012a, Fortran 90
 - wherever applicable
 - sampling distributions
 - size of the initial population of search points
-

Explanation of the calculated performances

- **stochastic methods**
 - no standard justification for the superior efficiency
 - no guarantees of optimality
 - cannot foresee the repeatability
 - possible explanation through the distinct features of each method
 - **CRSwCH, DE, SCE**
 - simple, rely on the difference of parameter vectors
 - hybrid, several different mechanisms to evolve the potential solution candidates
 - adaptive switching between different mechanisms
 - **PSO**
 - search is influenced by the points' neighborhoods
 - drive the population to local solutions
 - **SRES**
 - complex mutation stage
 - slow down the search procedure
 - **MIDACO**
 - Purely stochastic
 - **tdASA**
 - traditionally not suitable for continuous variables
 - **gblSolve**
 - expected low performance (deterministic algorithm)
-